

1 **The use of surfactants to enhance the solubility and stability of the**
2 **water-insoluble anticancer drug SN38 into liquid crystalline phase**
3 **nanoparticles**

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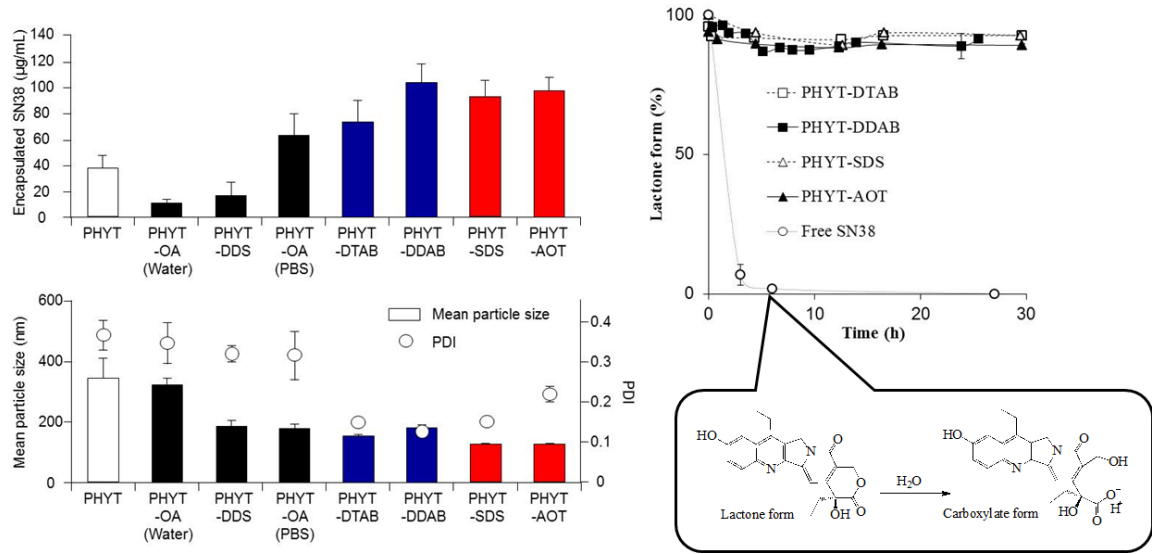
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Graphical abstract

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23 **Abstract**

24 Cubosomes were used to increase the aqueous solubility of the water insoluble
25 anticancer drug SN38. The results showed that the use of a common cubosome
26 formulation consisting of phytantriol (PHYT) as the matrix amphiphile
27 (PHYT-cubosome) led to a 6-fold increase in the solubility of SN38. However,
28 mean hydrodynamic diameter (D_H) and polydispersity index (PDI) of these
29 PHYT-cubosome particles were 345 ± 49 nm and 0.37 ± 0.05 , respectively, making
30 them unsuitable for intravenous applications. Several additives were
31 investigated to increase the solubility of SN38 and reduce the D_H and PDI values
32 of the resulting particles. Charged additives such as didodecyldimethyl
33 ammonium bromide (DDAB) and sodium dodecyl sulfate (SDS) led to
34 improvements in the physiochemical properties of the cubosomes. Notably, the
35 PHYT-DDAB and PHT-SDS cubosomes led to 15- and 14-fold increases in the
36 aqueous solubility of SN38, respectively. Moreover, the SN38 loaded into the
37 PHYT-DDAB and PHYT-SDS cubosomes was found to be highly stable, with
38 very little hydrolysis to its inactive acid form. In summary, the addition of
39 DDAB and SDS to PHYT-cubosome nanoparticle drug delivery systems not only
40 led to considerable improvements in their physiochemical properties, but also
41 enhanced the aqueous solubility of SN38 and increased its chemical stability.

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44 **Keywords:** cubosomes; poorly water-soluble drug; SN38; hydrolysis; chemical
45 stability

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47 Solubility is one of the most important factors affecting the absorption and
48 biodistribution properties of drugs. Poor aqueous solubility therefore represents
49 a considerable limitation during the development of therapeutic agents for oral
50 or intravenous administration, because water insoluble drugs struggle to achieve
51 the concentrations required to elicit therapeutic efficacy. Recent developments
52 in the field of nano-ordered drug delivery systems have allowed for the
53 successful encapsulation of a wide variety of anticancer drugs, leading to
54 considerable improvements in their targeting efficiency. These systems have
55 also led to a dramatic reduction in the side effects of these drugs (Murakami et
56 al., 2011) by increasing their solubility (Funakoshi et al., 2013; Barman et al.,
57 2014).

58 Cubosomes are lyotropic liquid crystalline phase nanoparticles that can be
59 prepared from amphiphiles, such as phytantriol (PHYT), which provide an inner
60 structure composed of lipid bilayers arranged in a contorted pattern around
61 adjacent water channels. This structure allows the lipid bilayer to act as a matrix
62 making the particles like a sponges. The properties of these systems make them
63 ideal candidates for the loading of highly hydrophobic drugs such as
64 7-ethyl-10-hydroxycamptothecin (SN38), which has a $\log P$ value of 3.37
65 (Thakur et al., 2010) (**Fig. 1**). SN38, which is formed as an active metabolite of
66 irinotecan (Zhang et al., 2004), is a potent anticancer drug with an IC_{50} value of
67 less than of 4 nM (Mariani et al., 2012). However, the clinical application of
68 SN38 has been limited by its poor aqueous solubility (7 $\mu\text{g}/\text{mL}$) and poor
69 stability, with its lactone ring being prone to hydrolysis under physiological
70 conditions to give the corresponding carboxylate, which is inactive (Zhang et al.,
71 2004). A recent successful attempt in increasing the solubility of SN38 was
72 reported using cationic materials with mesoporous silica (Bala et al., 2016).
73 Here, we envisioned that the use of additional excipients with either cationic or
74 anionic hydrophilic head, that have similar structural characteristics to PHYT
75 would allow us to increase the loading of SN38 into cubosome nanoparticles and
76 overcome both of those problems.

77 Firstly, we tried to load SN38, which was gifted from Yakult (Tokyo, Japan),
78 into a conventional cubosome formulation consisting of PHYT (Tokyo Kasei
79 chemicals, Tokyo, Japan) and Pluronic F127[®] (F127, BASF, Tokyo, Japan),
80 which was used as a steric stabilizer. SN38 was dissolved in a solution of 50 mg
81 of PHYT and 5 mg of F127 at 60–70 °C. One thousand, seven hundred and fifty
82 microliters of water was then added to the SN-38 solution, and the resulting
83 mixture was probe sonicated in pulse mode for 2 min. Two hundred microliters
84 of 10-times concentrated phosphate buffered saline (PBS) was added to the
85 sonicated solution, and the resulting mixture was sonicated for 0.5 min at 25 °C.
86 The final PBS solution contained NaCl, KCl, Na₂HPO₄ and KH₂PO₄ with the
87 following concentrations, 137, 2.7, 10 and 1.8 mM, respectively. The mixture
88 was centrifuged at 1000 ×g for 3 min at 25 °C to remove any unencapsulated
89 drug agglomerates or metal debris. The supernatant was collected and vortexed
90 for 10 min at 2500 rpm.

91 The concentration of SN38 in the PHYT cubosomes was measured using a
92 Shimadzu LC-2010C HT[®] HPLC system with a mobile phase consisting of a 1:1
93 (v/v) mixture of acetonitrile and an aqueous solution of 25 mM Na₂HPO₄ at a pH
94 of 7.4 (Xuan et al., 2006). The results revealed that the use of PHYT led to a
95 6-fold increase in the aqueous solubility of SN38 (39±8 µg/mL) (**Fig.2A**). The
96 mean hydrodynamic diameter (D_H) and poly dispersity index (PDI) were
97 determined by dynamic light scattering (Zetasizer Nano ZS[®], Malvern,
98 Worcestershire, UK). The results revealed that the suspension was polydispersed
99 with PDI and D_H values of 0.37±0.05 and 345±49 nm, respectively (**Fig.2B**),
100 indicating that this formulation would be unsuitable for intravenous application
101 because of the potential for enhanced permeability and retention effects
102 (Matsumura and Maeda, 1986).

103 To further increase the aqueous solubility of SN38 and improve the
104 physiochemical properties of the particles, we investigated the effects of adding
105 a variety of different additives to the initial SN38-PHYT mixture. A
106 PHYT/additive molar ratio of (1:13) was used in these experiments (Muir et al.,

107 2012). Several additives were evaluated, including didodecyl sulfoxide (DDS),
108 dodecyltrimethyl ammonium bromide (DTAB) and dioctyl sodium
109 sulfosuccinate (AOT), which were obtained from Tokyo Kasei Chemicals
110 (Tokyo, Japan). Oleic acid (OA) and didodecylammonium bromide (DDAB)
111 were purchased from Sigma Aldrich (Tokyo, Japan), and sodium dodecyl
112 sulfoxide (SDS) was obtained from Wako chemicals (Osaka, Japan).

113 Both PHYT-OA (water), prepared in deionized water, and PHYT-DDS were used
114 as neutral additive-based formulations. It has been reported that OA exists in its
115 un-ionized form when it is used as an additive in similar liquid crystalline systems.
116 It was therefore envisioned that OA would exist as a charge-neutral species under
117 salt-free conditions, with the ability to become anionic under more basic
118 conditions through deprotonation (Salentinig et al., 2010). Disappointingly,
119 however, both of these formulations led to negligible increases in the solubility of
120 SN38, with PHYT-OA (water) and PHYT-DDS leading to 1.5-fold (11 ± 3 $\mu\text{g/mL}$)
121 and 3-fold (18 ± 9 $\mu\text{g/mL}$) increases, respectively. Moreover, these formulations
122 were polydispersed with PDI values of 0.42 ± 0.05 and 0.33 ± 0.02 for PHYT-OA
123 (water) and PHYT-DDS, respectively. Based on the ionization of OA, we
124 subsequently investigated the effect of the nature of the additive head on the
125 properties of the system. Interestingly, we observed a 9-fold increase in the
126 solubility of SN38 (62 ± 16 $\mu\text{g/mL}$) in PHYT-OA formulation prepared in PBS, with
127 no noticeable difference in polydispersity properties of the suspension, which
128 gave a PDI value of 0.35 ± 0.07 . This result therefore highlighted the importance of
129 having charged additives for the loading of SN38 into these particles. To further
130 evaluate this hypothesis, we investigated several other charged additives.

131 The use of cationic additive-based formulations led a considerable increase in
132 the solubility of SN38, as exemplified by PHYT-DTAB and PHYT-DDAB
133 formulations, which resulted in 10-fold (74 ± 17 $\mu\text{g/mL}$) and 15-fold (104 ± 14
134 $\mu\text{g/mL}$) increases in the solubility, respectively. The resulting suspensions were
135 monodispersed with mean particle sizes of less than 200 nm, making them suitable
136 for future *in-vivo* applications. Furthermore, both PHYT-DTAB and PHYT-DDAB

137 formulations had PDI values of 0.15 ± 0.01 and 0.13 ± 0.02 , respectively. Anionic
 138 additive-based formulations showed similar trends to their cationic counterparts in
 139 terms of their ability to enhance the solubility of SN38, with PHYT-SDS and
 140 PHYT-AOT formulations leading to 13-fold ($93\pm 13 \mu\text{g/mL}$) and 14-fold (98 ± 10
 141 $\mu\text{g/mL}$) increases in the solubility. These formulations were also monodispersed
 142 with PDI values of 0.15 ± 0.01 and 0.22 ± 0.02 for the PHYT-SDS and PHYT-AOT
 143 particles, respectively. Furthermore, the mean particle sizes of the PHYT-SDS and
 144 PHYT-AOT particles were 125 ± 2 and 123 ± 11 nm, respectively. The charged
 145 additive-based systems showed higher SN38 loadings than the neutral systems,
 146 leading to higher aqueous solubility, regardless of the differences in the number of
 147 hydrophobic tails or the chemical structures of the tails. These results suggested
 148 that an interaction could have taken place in the lipid mixture prior to the addition
 149 of an aqueous solution or the sonication of the mixture. This interaction is
 150 supposedly manifested by the charged head of the surfactant electrostatically
 151 interacting with transient charges on the SN38 structure, such as the pyridine
 152 nitrogen or the phenol moiety, thereby facilitating the loading of the SN38
 153 molecules into the lipid bilayer of the cubic phase. Based on the SN38 loading,
 154 PDI and mean particle size characteristics of these systems, we selected the
 155 PHYT-DTAB, PHYT-DDAB, PHYT-SDS and PHYT-AOT formulations for further
 156 studies.

157 To gain a better insight into these systems, we evaluated their inner structures
 158 using small angle X-ray scattering (SAXS) analysis (NANO-Viewer system,
 159 Rigaku, Tokyo, Japan). These data allowed us to determine the space groups of
 160 these formulations based on the reciprocal spacing ratios of their three peaks, as
 161 mentioned elsewhere (Nakano et al., 2002). The cell parameter a (Å) was

162 calculated as follows: $a = \frac{\sqrt{h^2+k^2+l^2}}{Q*10}$

163 where Q is the norm of the scattering vector (nm^{-1}), and h , k and l are the
 164 Miller indices. Also, the channel size was calculated as mentioned elsewhere
 165 (Negrini et al., 2012) (**Table.1**). The details of all the formulations prepared in

166 the current study are shown in (**Fig.3A**). All of the formulations had the $Pn\bar{3}m$
167 cubic space group with peaks corresponding to miller indices of (110), (111),
168 (200) and (211). The PHYT-SDS formulation had an extra set of peaks with
169 reciprocals, indicating the presence of another space groups. Similar to the other
170 formulations, the first of these groups was determined to be the cubic space
171 group $Pn\bar{3}m$ with peaks corresponding to miller indices of (110), (111) and (211).
172 The second set of peaks corresponded to miller indices of (110), (200) and (211).
173 The absence a peak corresponding to (111) was attributed to the emergence of
174 the $Im\bar{3}m$ cubic space group. SAXS data concluded that the particles in these
175 formulations were cubosomes.

176 The second major issue concerning the use of SN38 is the susceptibility of its
177 lactone ring to hydrolysis under physiological conditions (pH 7.4), diminishing
178 the pharmacological activity of SN38 (Zhang et al., 2005). Under the
179 chromatographic conditions described above, we observed two distinct peaks
180 with retention times of 1.4 (carboxylate form) and 2.2 min (lactone form), for
181 samples composed of a 2:1 (v/v) mixture of acetonitrile and PBS (pH 7.4). Free
182 SN38 (i.e., SN38 not loaded into a cubosome formulation) was rapidly
183 hydrolyzed under these conditions to give the inactive carboxylate form almost
184 completely after 24 h. Furthermore, we only observed a small amount of lactone
185 by HPLC analysis (6.7% by peak area) after 3 h, with less than 0.1% remaining
186 after 24 h (**Fig. 3B**). However, SN38 showed much greater chemical stability
187 when it was loaded into a variety of cubosome formulations, as exemplified by
188 the PHYT-DTAB, PHYT-DDAB, PHYT-SDS and PHYT-AOT cubosomes, which
189 gave peak areas of 92.8, 91.7, 92.8 and 89.5% for the active lactone form after
190 26 h, respectively. These results suggested that the lactone ring of SN38 was
191 integrated into the cubic bilayer of the cubosome structure in these formulations,
192 making it much less susceptible to being attacked by water molecules. This kind
193 of interaction would most likely take place in the lipid mixture after the
194 sonication and self-assembly of the lipid bilayer. These results therefore provide
195 clear evidence that the loading of SN38 into cubosomes led to a considerable

196 increase in the chemical stability of this drug.

197 In conclusion, this study has demonstrated that the addition of charged
198 additives to PHYT-cubosomes loaded with the hydrophobic drug SN38 led to
199 considerable increases in the solubility of this system. Furthermore, the loading
200 of SN38 into these cubosome systems led to a dramatic increase in the
201 chemical stability of SN38 against hydrolysis at biological pH. The *in vivo*
202 evaluation of these systems in mouse models of human cancer would be of
203 considerable interest, since the cell membrane disrupting ability of PHYT- and
204 F127-based systems (Zhai et al., 2015) would show synergy effect with SN38 in
205 eliminating cancer cells.

206

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249

250 **Table captions**

251 **Table 1. Inner structure data of chosen formulations.** The properties of the
 252 inner structures were determined using small angle X-ray scattering

| Formulation | Space group | Cell parameter, a (Å) | Channel diameter (Å) |
|-------------|--------------|-------------------------|----------------------|
| PHYT | $Pn\bar{3}m$ | 65.20 ± 0.10 | 20.99 ± 0.03 |
| PHYT-DTAB | $Pn\bar{3}m$ | 78.84 ± 0.04 | 31.65 ± 0.02 |
| PHYT-DDAB | $Pn\bar{3}m$ | 74.80 ± 0.15 | 28.49 ± 0.06 |
| PHYT-SDS | $Im\bar{3}m$ | 104.97 ± 0.05 | 34.03 ± 0.02 |
| | $Pn\bar{3}m$ | 80.25 ± 0.16 | 32.76 ± 0.07 |
| PHYT-AOT | $Pn\bar{3}m$ | 70.90 ± 0.04 | 25.44 ± 0.01 |

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254

255 **Figure captions**256 **Figure 1. Chemical structures of the compounds used in this research.**

257

258 **Figure 2. Properties of the formulations prepared using phytantriol and**
259 **several different additives.** The solubility of SN38 in the different formulations
260 was measured by HPLC (a). The D_H and PDI results for the prepared formulations
261 were measured by DLS (b). Each point represents the mean \pm S.D ($n=3$). Samples
262 indicated with (*) showed statistically significant differences, $p<0.05$ in t -test, for
263 both of the vertical axes. Samples indicated with (#) showed statistically
264 significant differences, $p<0.05$ in t -test, for PDI only.

265

266 **Figure 3. Inner structure information and stability of the lactone form of**
267 **SN38.** The inner structure data of chosen formulations with peaks showing
268 corresponding miller indices and space group was obtained using SAXS (a). The
269 hydrolysis of the lactone form of SN38 in PBS (pH 7.4) (b). The dotted line
270 represents free SN38 without any cubosomes. The other lines represent SN38
271 encapsulated in cubosomes formulations with different additives, as indicated.
272 Each point represents the mean \pm S.D. ($n=3$). Schematic showing SN38
273 dispositioning within the lipid bilayer of one of the cubosomes formulations
274 (PHYT-SN38) where it is protected against hydrolysis.

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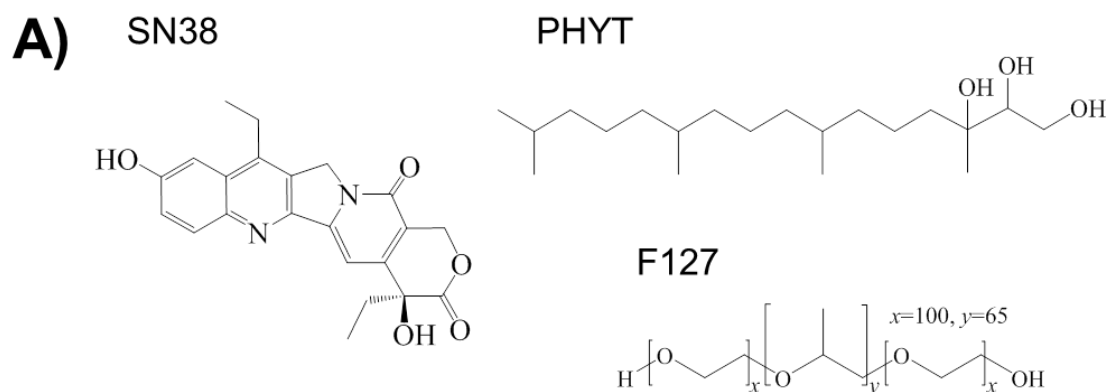
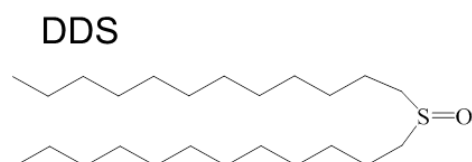
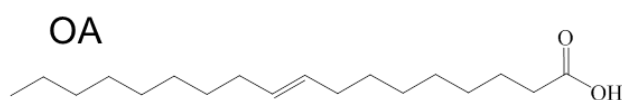
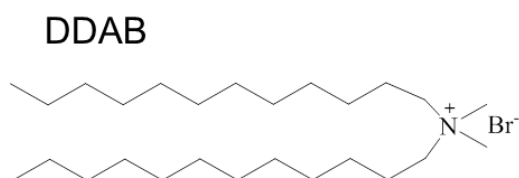
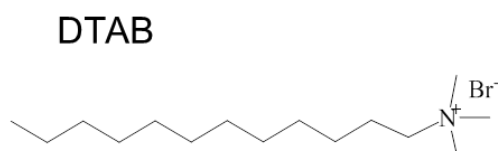
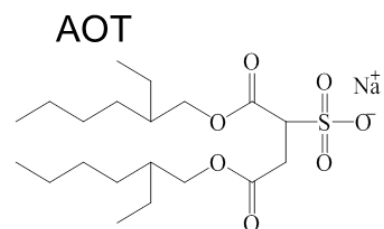
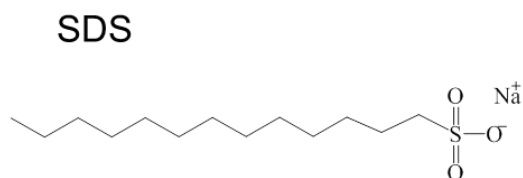
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Fig. 1

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**B) [Neutral additives]****[Cationic additives]****[Anionic additives]**

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Fig. 2

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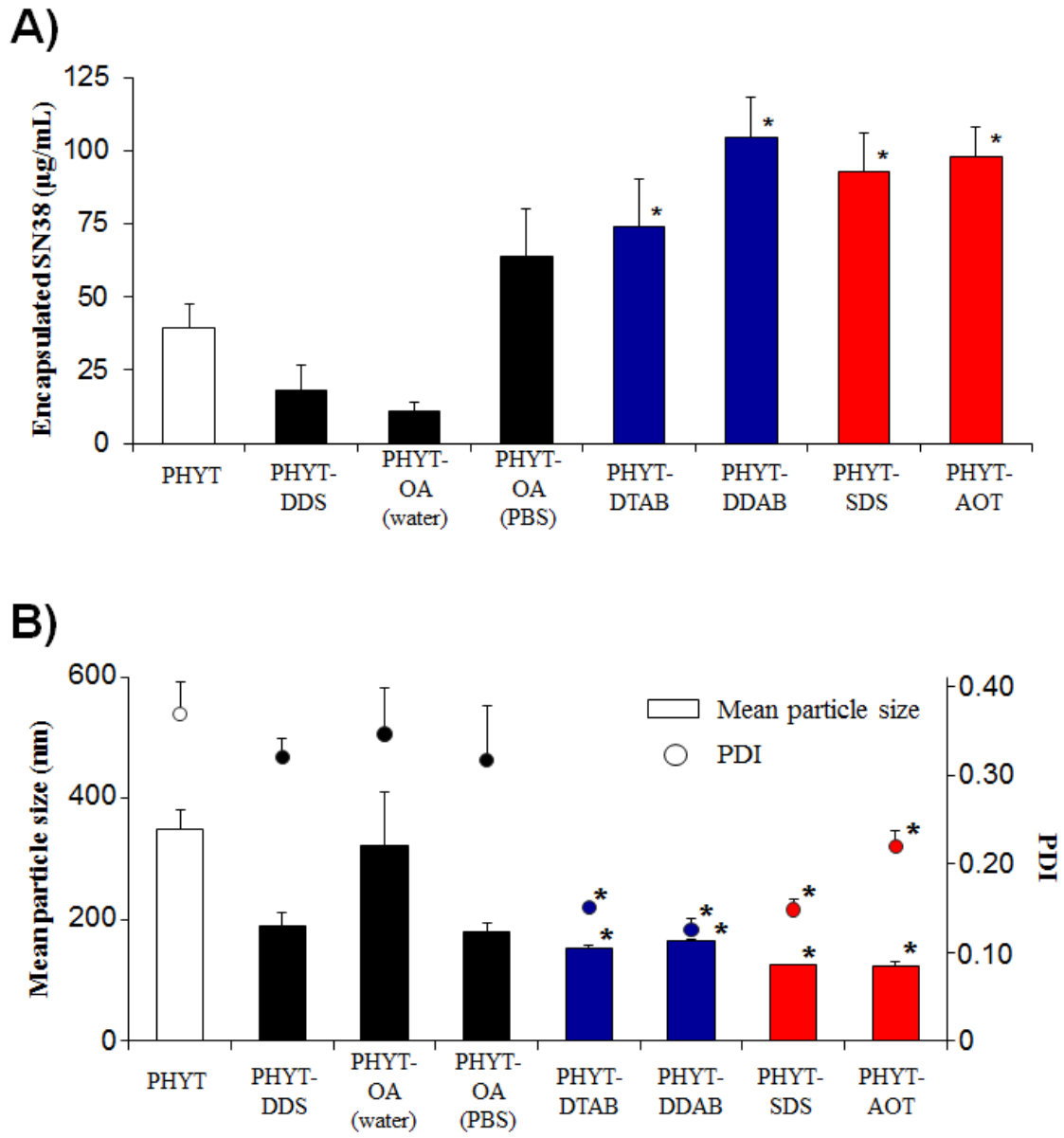


Fig. 3

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