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Application of water-insoluble polymers to orally disintegrating tablets treated by high-pressure carbon dioxide gas

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Abstract

The phase transition of pharmaceutical excipients that can be induced by humidifying or heating is well-known to increase the hardness of orally disintegrating tablets (ODTs). However, these conditions are not applicable to drug substances that are chemically unstable against such stressors. Here, we describe a system which enhances the hardness of tablets containing water-insoluble polymers by using high-pressure carbon dioxide (CO₂). On screening of 26 polymeric excipients, aminoalkyl methacrylate copolymer E (AMCE) markedly increased tablet hardness (+155 N) when maintained in a high-pressure CO₂ environment. ODTs containing 10% AMCE were prepared and treatment with 4.0 MPa CO₂ gas at 25°C for 10 min increased the hardness to +30 N, whose level corresponded to heating at 70°C for 720 min. In addition, we confirmed the effects of CO₂ pressure, temperature, treatment time, and AMCE content on the physical properties of ODTs. Optimal pressure of CO₂ gas was considered to be approximately 3.5 MPa for an AMCE formula, as excessive pressure delayed the disintegration of ODTs. Combination of high-pressure CO₂ gas and AMCE is a prospective approach for increasing the tablet hardness for ODTs, and can be conducted without additional heat or moisture stress using a simple apparatus.

39

Keywords: Orally disintegrating tablet, carbon dioxide, aminoalkyl methacrylate copolymer E

Abbreviations: AA, acrylic acid; AMCE, aminoalkyl methacrylate copolymer E; CMEC, carboxymethylethylcellulose; CO₂, carbon dioxide; EC, ethylcellulose; HPMCAS, hypromellose acetate succinate; MM, methyl methacrylate; ODT, orally disintegrating tablet; P_c , critical pressure; PEG, polyethylene glycol; PVA, polyvinyl alcohol; PVP, polyvinylpyrrolidone; PVP-VA, polyvinylpyrrolidone-co-vinyl acetate 64; SD, spray dried;

47 SEM, Scanning electron microscopy; T_c , critical temperature; T_g , glass transition temperature;
48 TEC, triethyl citrate; XPVP, crospovidone.

49

50 **1. Introduction**

51 Orally disintegrating tablets (ODTs) are representative dosage forms for oral drug
52 administration, and more than 100 products are now commercially available. ODTs
53 disintegrate in saliva and are easier to swallow than conventional tablets. They are therefore
54 expected to improve patient adherence (Koh *et al.*, 2008; Juul *et al.*, 2013), particularly in
55 children, the aged, and those with difficulties swallowing or under restricted water intake.
56 Zydis is a pioneer of this orally disintegrating dosage form (Seager, 1998), and is prepared by
57 freeze-drying suspensions or solutions containing active ingredients and excipients to make a
58 highly porous structured unit that results in rapid oral disintegration. However, Zydis has
59 several limitations compared with conventional tablets, such as a low manufacturing
60 efficiency and high cost. In addition, Zydis products are fragile and require peel-open blister
61 configurations, which are considered inferior in handling to the push-out blister
62 configurations of conventional tablets.

63 Several technologies to resolve these limitations have been developed and commercialized.
64 These include the application of a low compression force during the tableting process of wet
65 masses followed by drying (Tsushima, 2001), and tableting of dry masses followed by
66 heating or humidifying to increase hardness by enhancing the phase transition of excipients
67 (Kuno *et al.*, 2005; Mizumoto *et al.*, 2005; Sugimoto *et al.*, 2005). However, these methods
68 cannot be applied to active ingredients that are chemically unstable in conditions of high
69 temperature or moisture. We recently reported that microwave heating combined with wet
70 mass compression effectively enhances tablet hardness, but that the method was limited to
71 active ingredients with melting points higher than 110°C (Sano *et al.*, 2011, 2013 and 2014).

72 Another method is therefore required to raise tablet hardness without the stress induced by
73 heat and moisture. Other technologies that achieve sufficient hardness *via* high compression
74 force and use wicking agents to provide rapid disintegration have also been commercialized
75 (Okuda *et al.*, 2009 and 2012). However, these technologies are not universally applicable to
76 ODTs, as high compression force can damage the coating layer of micro-particles with active
77 ingredients, which are sometimes designed and formulated into ODTs to mask the bitterness
78 or control the release of active ingredients (Beckert *et al.*, 1996; Douroumis, 2011).
79 Technologies for ODTs which use a low compression force but enhance tablet hardness *via*
80 non-compression means remain technologically important.

81 To develop a new manufacturing process for ODTs, we focused on the use of pressurized
82 carbon dioxide (CO₂) as an alternative method for heating or humidifying, on the basis that
83 CO₂ is generally considered an inactive gas. High-pressure CO₂ acts as a plasticizer for
84 certain polymers by lowering their glass transition temperature (T_g), and this effect is
85 considered temporary because of the ease of removing CO₂ from polymers after
86 depressurization (Nalawade *et al.*, 2006). The plasticizing effect is due to the absorption of
87 CO₂ between polymer chains, which thereby increases the free volume and relaxes chain
88 entanglement, thus lubricating the inter-molecular space to reduce viscosity (Chiou *et al.*,
89 1985; Noto *et al.*, 2011). High-pressure CO₂ is used in the hot-melt extrusion process for
90 manufacturing solid dispersions, in which lowered T_g of polymers contributes to a more
91 efficient process with lower temperature, lower torque, and a higher extrusion rate (Verreck
92 *et al.*, 2005 and 2006; Lyons *et al.*, 2007). In addition, ODTs using pressurized CO₂ were
93 recently reported for the first time; in this process, tablets containing
94 polyvinylpyrrolidone-co-vinyl acetate 64 (PVP-VA) were pressurized with CO₂ to induce
95 phase transition of the polymer and form inter-granule bridging to increase tablet hardness
96 (Kobayashi *et al.*, 2013). However, the availability of a polymer that can enhance tablet

97 hardness more effectively than PVP-VA in the presence of CO₂ treatment has not been
98 reported. A higher content of water-soluble polymers such as PVP-VA would be considered
99 to delay disintegration of ODTs as they increase the viscosity of saliva during disintegration.
100 For this reason, the maximum content of water-soluble polymers in a hardness enhancement
101 system would be limited, and such polymers would be not always preferable as bridging
102 agents for ODTs. In fact, the addition of the water insoluble polymer ethylcellulose (EC) to a
103 formulation does not delay the disintegration of ODTs (Okuda *et al.*, 2012). The selection of
104 appropriate bridging agents, including water-insoluble polymers, to provide a better system
105 for enhancing the hardness of ODTs using high-pressure CO₂ therefore requires further
106 investigation.

107 Regarding manufacturing systems, the use of supercritical CO₂ at an industrial manufacturing
108 scale has been well-established, in food industries for example, but requires a
109 pressure-resistant container, condenser, and pump system to pressurize CO₂ for processing
110 tablets. Such a system would be excessively complicated and expensive to use as a
111 replacement for the heating and humidifying systems typically used in ODT production.
112 However, if pressurization in a high-pressure CO₂ system could be conducted at a lower
113 pressure than that of conventional liquefied CO₂ cylinders (ie. lower than approximately 6
114 MPa) at ambient temperature, the use of such a simplified system to produce ODTs might be
115 feasible. A system in which the CO₂ cylinders are connected only to a pressure-resistant
116 container the tablets are placed in, constitutes an alternative approach to heating and
117 humidifying. The production of ODTs with PVP-VA using CO₂ pressures lower than 6 MPa
118 at ambient temperature has been demonstrated (Kobayashi *et al.*, 2013). In that study,
119 however, more than 80% of the ODT composition consisted of a pre-mixed excipient, which
120 is a blend of several excipients and commercially available to achieve rapid disintegration.
121 Pre-mixed excipients have a complicated composition, however, and the effects of CO₂

122 treatment on them are unknown. Thus, investigating the effect of CO₂ treatment conditions
123 on the physical characteristics of ODTs would be better done using a simpler formula. Taken
124 together, these findings indicate that a better understanding of hardness enhancing systems
125 with plasticized polymers requires more thorough screening of bridging agents, including
126 water-insoluble polymers, and a closer examination of the effect of varying CO₂ conditions
127 on the physical properties of simpler formula ODTs.

128 Here, we screened a selection of polymeric excipients to evaluate their ability to increase
129 tablet hardness *via* treatment with high-pressure CO₂ gas at ambient temperature. In addition,
130 we also prepared ODTs using a more simplified formula with D-mannitol and conventional
131 disintegrant with an inter-granule bridging system involving the use of CO₂ gas and
132 water-insoluble polymer, and evaluated the effect of different treatment conditions on several
133 tablet properties.

134

135 2. Materials and methods

136 2.1. Materials

137 Direct compression grade D-mannitol (Parreck M 100) and magnesium stearate (Parreck LUB
138 MST) were purchased from Merck, Ltd. (Tokyo, Japan). Crystalline powder grade
139 D-mannitol (PEARITOL 50 C) was purchased from Roquette Japan K.K. (Tokyo, Japan).
140 Aminoalkyl methacrylate copolymer E (AMCE: Eudragit E PO), aminoalkyl methacrylate
141 copolymer RS (Eudragit RS PO and Eudragit RL PO), methacrylic acid copolymer LD
142 (Eudragit L100-55), methacrylic acid copolymer L (Eudragit L100), and methacrylic acid
143 copolymer S (Eudragit S 100) were purchased from Evonik (Tokyo, Japan). Hypromellose
144 acetate succinate (HPMCAS: AQOAT AS-HF), low-substituted hydroxypropyl cellulose
145 (L-HPC NBD-022), and hypromellose (TC-5 E) were purchased from Shin-Etsu Chemical
146 Co., Ltd. (Tokyo, Japan). Carboxymethylethylcellulose (CMEC) was purchased from Freund
147 Corporation (Tokyo, Japan). EC (ETHOCEL Standard 7 FP Premium) was purchased from
148 Dow Chemical Company (Tokyo, Japan). White shellac (dried white shellac) was purchased
149 from The Japan Shellac Industries, Ltd. (Osaka, Japan). Polyvinyl
150 acetate/polyvinylpyrrolidone (Kollidon SR), crospovidone (XPVP: Kollidon CL-F),
151 polyvinylpyrrolidone (PVP: Kollidon 30), PVP-VA (Kollidon VA 64 and Kollidon VA 64
152 Fine), polyethylene glycol and polyvinyl alcohol graft copolymer (PEG-PVA graft
153 copolymer: Kollicoat IR) and polyvinyl caprolactam-polyvinyl acetate-polyethylene glycol
154 graft copolymer (Soluplus) were purchased from BASF Japan, Ltd. (Tokyo, Japan).
155 Croscarmellose sodium (Kiccolate ND-2HS) and partly pregelatinized starch (PCS) were
156 purchased from Asahi Kasei Chemicals Corp. (Tokyo, Japan). Carmellose (NS-300) and
157 carmellose calcium (E.C.G-505) were purchased from Gotoku Chemical Co., Ltd. (Tokyo,
158 Japan). Sodium carboxymethyl starch (Primojel) was supplied by DFE Pharma (Tokyo,
159 Japan). Cornstarch (Nisshoku Cornstarch, JP) was purchased from Nihon Shokuhin Kako Co.,

160 Ltd. (Tokyo, Japan). Hydroxypropylcellulose (NISSO HPC-SSL) was purchased from
161 Nippon Soda Co., Ltd. (Tokyo, Japan). Polyvinyl alcohol/acrylic acid/methyl methacrylate
162 copolymer (PVA/AA/MM copolymer: POVACOAT Type SP) was purchased from Nisshin
163 Kasei Co., Ltd. (Osaka, Japan). Carboxyvinyl polymer (Carbopol 940) was purchased from
164 The Lubrizol Corporation (Wickliffe, OH, USA). Triethyl citrate (TEC) was purchased from
165 Tokyo Chemical Industry Co., Ltd. (Tokyo, Japan). All reagents used were of analytical
166 grade and available from commercial sources, and all solutions were prepared with deionized
167 water.

168

169 2.2. Preparation of tablets

170 2.2.1. Preparation of tableted samples for polymer screening study

171 Various polymeric excipients were formulated, and a portion of the aggregated materials was
172 ground in a mortar before use. Dried white shellac was pulverized using a pin mill (100 UPZ
173 Fine Impact Mill; Hosokawa Micron Corporation, Osaka, Japan) before use. EC and triethyl
174 citrate (weight ratios: 9/1 and 7.5/2.5) were dissolved in ethanol, and the ethanol solutions
175 were spray dried (SD) using a Mini Spray Dryer B-290 (Nihon BUCHI K.K., Tokyo, Japan)
176 to obtain EC/TEC (9/1) SD and EC/TEC (7.5/2.5) SD.

177 D-mannitol as direct compression grade, polymeric excipients, or the SDs described above
178 and magnesium stearate were weighed and mixed in 70-mL plastic bottles to prepare blends
179 for compression on a 10-g scale, according to the formulation in **Table 1**. The polymeric
180 excipients and SDs are shown in **Table 2**. Blends were weighed for each tablet and
181 compressed using a test apparatus (Autograph AGS-20 kNG; Shimadzu, Kyoto, Japan), fitted
182 with a round face punch 8.5 mm in diameter. Tablet weight and compression force were
183 adjusted for each formulation to ensure that tablet hardness was 20 ± 2 N and thickness was
184 4.0 ± 0.30 mm.

185

186 2.2.2. Preparation of tableting samples of ODTs (Form A and B)

187 Crystalline powder grade D-mannitol was granulated using top-spraying binder (PVP or
188 PVP-VA) solution (10% [w/w] concentration) with a fluidized-bed granulator (FLO-1;
189 Freund Corporation, Tokyo, Japan) at 420-g scale. AMCE and magnesium stearate were
190 sieved with a 710- μ m screen before use. These excipients and intact XPVP were then blended
191 with the granules in a plastic bag for 1 min. The blended components were compressed using
192 a rotary tableting machine (EX10; Hata Iron Works Co., Ltd., Kyoto, Japan) with
193 8.5-mm-diameter round face punches. Tablets were compressed at 1-2 kN/punch to obtain
194 approximately 10 N of tablet hardness. The formulations manufactured by this procedure are
195 shown in **Table 3** (A-1, A-2 and B-1).

196 To confirm the effect of AMCE content in formulations, granules (B-1) were blended with
197 sieved AMCE, XPVP and sieved magnesium stearate in a plastic bottle for 1 min at a 10 g
198 scale, according to the formulation shown in **Table 3** (B-2, B-3 and B-4). Blends were
199 weighed for each tablet and compressed using a compaction test apparatus (Autograph
200 AGS-20 kNG; Shimadzu, Kyoto, Japan) with a compression force of approximately 1
201 kN/punch with a round face punch of 8.5 mm in diameter.

202

203 2.2.3. Treatment of samples by high-pressure CO₂ gas

204 Some polymeric excipients or tablets were treated with high-pressure CO₂ gas using the
205 apparatus shown in **Fig. 1**. This process was conducted in a 50-mL pressure-resistant
206 container (EV series; JASCO, Tokyo, Japan). Temperature in the container was monitored
207 using a thermometer TI-2068 (JASCO), the detector of which was tightly inserted into the
208 container. The container had two attached flow channels for inlet and outlet CO₂ gas. The
209 inlet line connected to a 7-m³ cylinder of liquefied CO₂ (non-siphon type; Tomoe Shokai Co.,

210 Ltd., Tokyo, Japan). The outlet led to an automatic back-pressure-regulating valve BP-2080
211 (JASCO) that regulated the pressure in the container and line by releasing excess CO₂ when
212 the pressure exceeded the target according to a preset program. Temperature was controlled
213 by setting the container and CO₂ lines in the CO-2060 thermostatic chamber (JASCO). In this
214 treatment process, tablets were set in the container with temperature controlled at 15–45°C,
215 which was then closed tightly. CO₂ gas filled the container and the pressure was controlled
216 from 1 to 6 MPa by BP-2080. Pressure and temperature were kept constant for 5–360 min,
217 and treated samples were obtained after releasing CO₂ gas at a rate of 1 MPa/min. Pressure,
218 temperature, and time were altered according to study conditions.

219

220 2.2.4. Treatment of samples by heating

221 In some experiments, tablets were heated as a substitution for high-pressure CO₂ gas
222 treatment. Regarding the polymer screening study, tablets with AMCE, CMEC, XPVP,
223 PEG-PVA graft copolymer or PVA/AA/MM copolymer were heated in an oven (WFO-510;
224 Tokyo Rikakikai Co., Ltd., Tokyo, Japan) without exposure to high-pressure CO₂ gas
225 treatment. Tablets on stainless mesh were processed at 80°C for 840 min to obtain
226 heat-processed samples. Formula A-1 tablets were heated at 70°C for 45–720 min in the same
227 manner as above. Some polymeric excipients were also heated at 70°C for 45–840 min on a
228 glass dish to observe scanning electron microscopy images.

229

230 2.3. Characterization of samples

231 2.3.1. Tablet hardness

232 Tablet hardness was defined as the force required to break a tablet by radial static
233 compression. Tablet hardness was determined using a tablet hardness tester (Model 6D; Dr.
234 Schleuniger Pharmatron, Thun, Switzerland). Measurements were repeated twice in the

235 polymer screening study, while other experiments were repeated five times. Standard
236 deviation was also calculated.

237

238 2.3.2. Tablet thickness

239 Tablet thickness was measured at the center of the tablet using a micrometer with a precision
240 of 0.01 mm (Digimatic Indicator; Mitsutoyo Corporation, Kanagawa, Japan). Measurements
241 were repeated twice in the polymer screening study, while other experiments were repeated
242 five times. Standard deviation was also calculated.

243

244 2.3.3. Disintegration time

245 Disintegration time was measured using a rapid disintegration tablet tester (Tricorptester;
246 Okada Seiko Co., Ltd., Tokyo, Japan) (Yoshita *et al.*, 2013). Tests were conducted with
247 tablets axially sandwiched between two stainless meshes (20 g of upper mesh), and purified
248 water ($37 \pm 1^\circ\text{C}$) was dropped on the upper mesh at a constant rate of 6 mL/min to
249 disintegrate the tablet. Disintegration time was defined as the time from the first droplet to
250 when the two meshes made complete contact after tablet disintegration. This measurement
251 was conducted using sensory recognition. The disintegration time of three separate tablets
252 was measured, and the mean and standard deviation were calculated.

253

254 2.3.4. Scanning electron microscopy (SEM)

255 SEM images of some polymeric excipients were obtained using a scanning electron
256 microscope (VHX-2000; Keyence, Osaka, Japan). Powdery excipients or agglomerated
257 excipients after heating or CO₂ pressurization were immobilized on a metal base with
258 adhesive tape.

259

260 *2.4. Statistics*

261 Statistical analyses were performed using Student's t-test. $p < 0.05$ was considered
262 statistically significant.

263

264 3. Results and Discussion

265 3.1. Effect of polymeric excipients on increased tablet hardness by high-pressure CO₂ gas

266 Screening of conventional polymeric excipients used for oral dosage forms was conducted to
267 confirm which were the most effective in enhancing tablet hardness *via* high-pressure CO₂
268 gas treatment. **Table 2** shows the various polymeric excipients used to prepare tablets that
269 were treated with high-pressure CO₂ gas at 6.0 MPa/25°C/45 min. Pressure was fixed at 6.0
270 MPa because this value was considered the near upper limit of the gaseous state of CO₂
271 ($T_c=304.15$ K, $P_c=7.38$ MPa) that could be achieved by releasing pressure from conventional
272 cylinders of liquefied CO₂ without using a condenser. **Table 2** also shows changes in tablet
273 hardness and thickness after high-pressure CO₂ treatment. AMCE, HPMCAS, and PVP-VA
274 increased tablet hardness by more than 50 N after treatment (AMCE: +155 N, HPMCAS:
275 +65N, and PVP-VA: +69 N), while D-mannitol and magnesium stearate, without any other
276 polymeric excipients, increased hardness by only 2 N. This suggests that the increase in
277 hardness with the three formulations was due to the effective phase transition of polymeric
278 excipients induced by high-pressure CO₂ gas treatment and the increase in the resultant
279 inter-granule bridging formed by rubber-state polymers. This notion was supported by the
280 SEM images in **Fig. 2**, in which the particle shapes of AMCE, HPMCAS and PVP-VA were
281 lost or deformed to make inter-particle bridging after CO₂ treatment at 6.0 MPa/25°C/45 min.
282 In contrast, CMEC did not show any changes. These findings were well correlated with the
283 results of tablet hardness testing, in which AMCE, HPMCAS and PVP-VA showed increased
284 hardness but did not CMEC. Our results with the PVP-VA formulation were comparable to
285 those in a previous report (Kobayashi *et al.*, 2013). These findings suggested that
286 water-insoluble polymers such as AMCE and HPMCAS are suitable candidates as bridging
287 agents for ODTs. In the SEM images, the morphology of AMCE was significantly changed
288 compared with that of PVP-VA under the same pressure conditions, indicating that AMCE

289 enhances tablet hardness with lower CO₂ pressure. According to the vendor's information,
290 the T_g values of PVP-VA and AMCE were 101°C and 45°C, respectively. This lower T_g of
291 AMCE might explain why it was more significantly plasticized than PVP-VA under the same
292 CO₂ gas treatment. In addition, the difference in physical strength of the bridging polymers
293 themselves might also affect tablet hardness. Our findings suggest that AMCE, an insoluble
294 polymer in aqueous solvents at pH ≥ 5 , might be a promising bridging agent for ODTs that
295 utilize CO₂.

296 To confirm the effect of T_g of bridging polymers on the efficiency of hardness enhancement
297 using high-pressure CO₂, EC was spray-dried with TEC as plasticizer and tablets containing
298 EC/TEC SD were treated with CO₂. In general, the T_g of polymers is decreased by the
299 addition of plasticizers such as TEC (Repka *et al.*, 1999). **Table 2** indicates that the
300 formulation containing EC/TEC (9/1 and 7.5/2.5) SD showed a marked increase in tablet
301 hardness (+67 and +75 N, respectively) after CO₂ pressurization. In contrast, intact EC
302 showed a smaller increase (+11 N) in hardness after the process. Kojima and Nakagami
303 demonstrated that the addition of 10% and 22.7% TEC decreased the T_g of EC from
304 approximately 130°C to 80°C and 50°C, respectively, and that the minimum film-forming
305 temperature of EC corresponded with T_g (2002). In the current CO₂ system, these data
306 suggest that the T_g of the bridging agent is an important factor in determining the increment
307 level of hardness and that the addition of a plasticizer can enhance tablet hardness by
308 decreasing T_g , even if the bridging polymer cannot be well plasticized by high-pressure CO₂
309 gas.

310 Tablets were also processed at 80°C for 840 min as a substitution for high-pressure CO₂ gas
311 treatment using AMCE, CMEC, XPVP or PEG-PVA graft copolymer or PVA/AA/MM
312 copolymer. Regarding AMCE, because this polymer increases tablet hardness at temperatures
313 exceeding the T_g (Suzuki, 2006), its ability to increase tablet hardness by the heating method

314 and CO₂ method should be compared. **Table 2** shows a marked increase in hardness for
315 AMCE (+109 N) by heating at 80°C, which is likely attributable to the phase transition of
316 AMCE, as supported by the previous report. This indicates that CO₂ treatment of the AMCE
317 formulation at 6.0 MPa/25°C/45 min can increase tablet hardness more effectively (+155 N)
318 than heating at 80°C/840 min. While with the CMEC, XPVP, and PEG-PVA graft copolymer
319 and PVA/AA/MM copolymer increased tablet thickness by more than 0.2 mm after CO₂ gas
320 treatment, representing a nearly 20-fold increase compared with the control sample (+0.01
321 mm), the AMCE formulation markedly increased hardness without any change in thickness.
322 The increase in tablet thickness might be attributable to the swelling of polymeric excipients
323 by CO₂ treatment (Guadagno and Kazarian, 2004, Pasquali *et al.*, 2008). To estimate whether
324 the thickness increase confirmed in some formulas was specific to CO₂ treatment, the effect
325 of the CO₂ and heating processes on thickness was compared for CMEC, XPVP, and
326 PEG-PVA graft copolymer and PVA/AA/MM copolymer. For the PEG-PVA graft
327 copolymer and PVA/AA/MM copolymer formulations, heated samples were thicker (+0.24
328 mm) than or almost equal (−0.02 mm) to those with CO₂ gas treatment. The change in
329 thickness of these samples after CO₂ gas treatment might therefore not be solely due to CO₂
330 gas treatment. Thickness generally increases after tableting due to the plastic recovery of
331 excipients (Sarkar *et al.*, 2014) or moisture absorption by disintegrants. **Table 2** also shows a
332 lower increase in thickness (+0.07 and +0.01 mm) in tablets with super disintegrants
333 (Kiccolate ND-2HS and Primojel), which might suggest that the thickness increase in the
334 PEG-PVA graft copolymer and PVA/AA/MM copolymer formulations during CO₂ gas
335 treatment or heating was not primarily due to moisture absorption, but rather due to the
336 plastic recovery of polymers after tableting. In contrast, thickness after CO₂ treatment
337 increased by 0.33 mm for XPVP and 0.32 mm for CMEC, whereas thicknesses after heating
338 increased by 0.12 mm for both formulas. These findings suggest that XPVP and CMEC

339 might swell in response to high-pressure CO₂ gas, which would increase tablet thickness and
340 lower tablet hardness after CO₂ gas treatment (**Table 2**). These findings stress the importance
341 of excipient selection for use with high-pressure CO₂ gas systems for ODTs, wherein some
342 excipients would increase hardness whereas others would decrease it.

343

344 *3.2. Time course of tablet hardness and thickness by heating and pressurizing with CO₂ gas*

345 **Table 2** shows that high-pressure CO₂ gas treatment at 25°C might increase tablet hardness
346 *via* induction of phase transition of AMCE more effectively than that occurring following
347 heating at 80°C. To confirm this in more detail, A-1 formulations of ODTs were heated at
348 70°C and A-2 formulations were treated with CO₂ gas at 4.0 MPa/25°C (**Table 3**). Here, we
349 selected 70°C as heating temperature because 80°C would be too high considering the T_g of
350 AMCE. **Fig. 2** indicates that AMCE was well plasticized with CO₂ at 4.0 MPa, and this
351 condition was therefore selected for this experiment. The time courses of tablet hardness and
352 thickness for each treatment were evaluated (**Fig. 3**). The endpoint was the attainment of a
353 hardness plateau, or 720 min, corresponding to one-night treatment, whichever occurred first.
354 Both treatments significantly increased tablet hardness in a time-dependent manner, in which
355 CO₂ gas treatment at ambient temperature reached more than 40 N within 10 min of
356 treatment whereas heating at 70°C required 720 min (**Fig. 3a**). Formula A contained XPVP,
357 which swelled in response to CO₂ gas treatment, as mentioned above. **Fig. 3b** shows the time
358 course of change in tablet thickness: high-pressure CO₂ gas treatment significantly increased
359 thickness for all time points compared with levels before treatment (shown as sample at 0
360 min), whereas heating did not affect thickness. Hardness of tablets measured at 10 min of
361 CO₂ gas treatment was closely similar to that at 720 min of heating, and only the former
362 exhibited a significant increase in thickness. This implies that increased thickness was
363 specific to the high-pressure CO₂ gas system. Both A-1 and A-2 formulas contain D-mannitol,

364 PVP, AMCE and magnesium stearate (**Table 3**), and **Table 2** shows that these excipients did
365 not increase tablet thickness following CO₂ gas treatment. We therefore propose that XPVP is
366 the main reason why only A-2 exhibited a significant increase in thickness but not with
367 heating. Previous reports (Guadagno and Kazarian, 2004, Pasquali *et al.*, 2008) have
368 indicated that swelling of polymers can occur due to CO₂ absorption, which would support
369 XPVP swelling in response to high-pressure CO₂ gas. Taken together, these results for the
370 AMCE formula suggest that the CO₂ method under ambient temperature enhances tablet
371 hardness more rapidly than the heating method and increases thickness in a
372 formulation-dependent manner.

373 Although the processing time of the heating method could be reduced by using higher
374 temperatures, such a time reduction would not be preferable from the perspective of thermal
375 stress on drug substances. The likely reason for the more rapid increase in tablet hardness
376 with CO₂ gas treatment is explained by **Fig. 4**. CO₂ treatment at 4.0 MPa/25°C/120 min
377 changed AMCE morphologically and its original particle shape was lost completely. In
378 contrast, AMCE particles were significantly identified at 70°C/120 min, and morphological
379 change was not still as significant at 70°C/840 min as with the CO₂ treatment. These
380 differences appear to make CO₂ treatment at 4.0 MPa/25°C more effective at increasing tablet
381 hardness than heating at 70°C.

382

383 *3.3. Effect of treatment conditions of CO₂ gas on the physical properties of ODTs*

384 Regarding the plasticizing effect of pressurized CO₂ on polymers, the melting temperature of
385 PEG 1500 has been shown to decrease in a manner that was dependent upon CO₂ pressure
386 (Pasquali *et al.*, 2008). In a CO₂-based tablet hardness enhancement system which uses
387 plasticized polymer, pressure of CO₂ affects tablet hardness (Kobayashi *et al.*, 2013). We
388 therefore considered that CO₂ pressure is a key factor, and its effect on the physical properties

389 of ODTs in the hardness-enhancing system with AMCE was examined. ODTs were prepared
390 in accordance with the B-1 formula shown in **Table 3**, and tablets were processed at various
391 pressures, temperatures, and processing times using high-pressure CO₂ gas. The B-1 formula
392 contains PVP-VA as the binder in the granulating process and XPVP as disintegrant. These
393 were selected from our preliminary studies on the basis of the disintegration properties of
394 ODTs (data not shown). It is known that tablets containing PVP-VA have increased hardness
395 following high-pressure CO₂ treatment. To evaluate the effect of PVP-VA in granules on
396 hardness of the B-1 formula, tablets prepared with B-1 granules and magnesium stearate were
397 treated with high-pressure CO₂ gas (4.0 MPa/25°C/45 min), and an increase in hardness of +3
398 N was confirmed (data not shown). This slight increase in hardness produced by PVP-VA in
399 B-1 granules was likely due to the low content of PVP-VA (2%) in the granules. The effect of
400 PVP-VA in B-1 granules on tablet hardness was therefore considered negligible.

401

402 3.3.1. Effect of pressure of CO₂ gas and processing temperature on ODTs

403 The effect of CO₂ gas pressure and temperature on the physical properties of B-1 tablets was
404 evaluated with a constant processing time of 45 min (**Fig. 5**). Considering the T_g
405 (approximately 48°C) of AMCE, 45°C was set as highest temperature condition to ensure
406 testing of whether AMCE was plasticized by CO₂, and not by heating. **Fig. 5a** shows
407 increased tablet hardness in a CO₂ pressure-dependent manner for all temperatures. There
408 were significantly higher increases in hardness for treatment at 45°C than 15°C under CO₂
409 pressures lower than 4.0 MPa, although this tendency was not observed at 4.0 MPa or higher.
410 In this system, plasticization of ACME is key to the enhancement of hardness, and would be
411 affected by CO₂ pressure and temperature. AMCE forms inter-granule bridging when
412 temperature conditions surpass the T_g , which is reduced by high-pressure CO₂ gas. At 2.0–3.0
413 MPa, the reduction in T_g by CO₂ gas might not be drastic, and the temperature effect on tablet

414 hardness might therefore be significant. In contrast, at pressures exceeding 3.0 MPa, gaps in
415 hardness between temperature conditions were not as large as those at 2.0–3.0 MPa. As
416 confirmed in **Fig. 3**, 4.0 MPa/25°C of CO₂ gas increased hardness more rapidly than heating
417 at 70°C, which implies that the plasticizing effect at 4.0 MPa/25°C corresponded to heating at
418 temperatures higher than 70°C. AMCE was therefore considered to be drastically plasticized
419 by CO₂ gas at pressures exceeding 3.0 MPa, even at 15°C, and no significant temperature
420 effects observed.

421 **Fig. 5b** shows the same experiments as **Fig. 5a**, except that the horizontal axis corresponds to
422 CO₂ density, not pressure (Span and Wagner, 1996). CO₂ pressure is correlated with CO₂
423 density and likely an important factor influencing the dissolution of polymers, as CO₂ volume
424 is changed in a temperature-dependent manner and CO₂ densities can be different, even under
425 the same pressure conditions. As density is an output factor that is calculated from pressure
426 and temperature, the monitoring of pressure during the CO₂ treatment process might be
427 simpler and preferable to that of density. **Fig. 5b** shows that CO₂ density has a similar effect
428 to CO₂ pressure. Our results suggest that tablet hardness can be controlled by CO₂ pressure
429 (or density) and temperature in this system.

430 We also confirmed that tablet thickness increased in a pressure-dependent manner at 15, 25,
431 35, and 45°C (**Fig. 5c**). XPVP was considered the main component that increased the
432 thickness of tablets (**Table 2**). Results indicated that the increase in thickness was not as
433 temperature-dependent as hardness, which might suggest that the swelling properties of
434 XPVP are not dependent on temperature. Furthermore, although the influence of temperature
435 on the disintegration properties of ODTs was not significant, they were effected by pressure:
436 namely, the 4.0 MPa condition tended to delay disintegration time in comparison with 3.5
437 MPa or lower conditions (**Fig. 5d**). We do not expect that tablet disintegration time would
438 increase markedly (> 120 s at 4.5 MPa or higher) for all temperature conditions (data not

439 shown), but do not consider that the longer disintegration time was simply caused by excess
440 tablet hardness, as no drastic increase in hardness was observed at pressures of 4.0–4.5 MPa.
441 XPVP was considered to swell during treatment with high-pressure CO₂ gas. We also
442 confirmed that the disintegrating property and particle size of XPVP did not change
443 following high-pressure CO₂ gas treatment (data not shown). This implies that the swelling of
444 XPVP is tentative during the process and reversible in response to depressurization. In the
445 hardness-enhancing process of B-1 tablets by CO₂ gas, excess bridging between AMCE and
446 XPVP might explain why the disintegrating property of XPVP deteriorated at pressures of 4.5
447 MPa or higher. However, our results indicate that this phenomenon is not so simple. As
448 shown in **Table 4**, the B-4 formula (12.5% AMCE) showed a hardness of 57 N, while it
449 disintegrated within 15 s. The hardness of higher than 50 N with the B-4 formula was
450 achieved by combining a higher amount of AMCE with a CO₂ pressure of lower than 4.5
451 MPa. These findings suggest that the delayed disintegration under higher pressure conditions
452 is not caused only by the excess bridging of AMCE. At higher pressure conditions, phase
453 transition of AMCE and swelling of XPVP would be significant and occur in parallel,
454 potentially delaying disintegration, as melted AMCE is able to bridge with swelled XPVP.
455 The interaction might disturb XPVP recovery from the swelling state to inactivate the
456 disintegrating property. We also confirmed that the B-1 formula without XPVP took longer
457 than 120 s to disintegrate (data not shown), indicating that XPVP is necessary to the rapid
458 disintegration property of the B-1 formula and that inactivation of XPVP would occur at 4.5
459 MPa or higher. A key factor of this ODT system, in which AMCE is plasticized by CO₂ gas,
460 is to control CO₂ pressure so as not to reduce the disintegrating property of XPVP. These
461 findings might prove to be a disadvantage when applying water-insoluble polymers as
462 bridging agents in hardness-enhancing systems using CO₂. In contrast, ODTs using PVP-VA
463 as a hardness enhancer disintegrated within 30 s after treatment by 8.0 MPa CO₂ (Kobayashi

464 *et al.*, 2013). This might be attributable to differences in the formulation of samples, given
465 that we used simple formulations containing XPVP as a disintegrant whereas Kobayashi *et al.*
466 applied a pre-mixed excipient for easy disintegration. It would be interesting to understand
467 the different effects of water-soluble and -insoluble polymers on the physical properties of
468 ODTs produced by hardness enhancement systems using CO₂.

469

470 3.3.2. Effect of pressurized CO₂ gas processing time on ODTs

471 We then evaluated the effect of treatment time on the physical properties of ODTs. B-1
472 tablets were treated with CO₂ gas at 3.0, 3.5, 4.0 and 5.0 MPa at a constant temperature of
473 25°C with processing times of 5–360 min, and the hardness, thickness, and disintegration
474 time of ODTs were tested (**Fig. 6**). As shown in **Fig. 5**, tablet hardness increased by less than
475 +10 N under the 2.0 MPa condition, whereas the increase between 3.0–4.0 MPa was more
476 drastic in the tested range. We therefore excluded the 2.0 MPa condition in the next study and
477 instead 0.5-MPa steps between 3.0–4.0 MPa. Results showed that the highest-pressure
478 condition (5.0 MPa) enhanced hardness by +36 N after only 5 min of treatment (**Fig. 6a**) and
479 that tablets disintegrated within 30 s (**Fig. 6c**), which was considered acceptable for ODTs.
480 Comparison of four different CO₂ gas pressure conditions showed that higher pressure
481 achieved higher tablet hardness with the same treatment time. Tablet hardness following
482 treatment with a range of CO₂ pressures for 45 min was as follows: 3.0 MPa (23 N), 3.5 MPa
483 (33 N), 4.0 MPa (44 N), and 5.0 MPa (52 N). These results suggest that tablet hardness can
484 be controlled by optimizing CO₂ gas pressure and processing time under a constant
485 temperature condition of 25°C. As mentioned above, an increase in hardness of more than 30
486 N was confirmed using treatment at 5.0 MPa/25°C/5 min (**Fig 6a**). This implies that the
487 phase transition of AMCE by CO₂ gas occurred within a remarkably short time. Other
488 pressure conditions also tended to enhance tablet hardness within the first 10 min, followed

489 by moderate increases. This suggests that the hardness-enhancing process might consist of
490 two different phases. First, AMCE transits from glass to rubber to increase hardness and then
491 diffuses into the voided space of the tablet, enlarging its contact area with surrounding
492 granules. The diffusion phase might result in more moderate increases in tablet hardness,
493 although higher pressures induce more marked increases in the diffusion phase when the
494 hardness profiles at 3.0 MPa were compared with those at 4.0 MPa within 30–60 min (**Fig**
495 **6a**). This might suggest that mobility of AMCE in the rubber state during CO₂ gas treatment
496 is determined by pressure, albeit that a more detailed examination is required.

497 Regarding tablet thickness (**Fig. 6b**), a time-dependent increase was also observed, but this
498 was not as significant as hardness under the lower pressure conditions of 3.0 and 3.5 MPa. As
499 discussed above, increased thickness is likely attributable to XPVP. Furthermore, increased
500 hardness and thickness could be induced by different mechanisms, explaining why hardness
501 was significantly increased under low-pressure conditions while thickness was not. We
502 confirmed that 4.5 MPa treatment for 45 min resulted in a significant delay in the
503 disintegration properties of tablets (3.3.1., data not shown). A significant delay in
504 disintegration (>120 s) was confirmed using 4.0 MPa for longer than 60 min and 5.0 MPa for
505 longer than 5 min (data not shown), and a tendency for delayed disintegration was observed
506 at 3.5 MPa for 360 min (**Fig. 6c**). However, high pressure conditions can also make ODTs
507 disintegrate within 20 s by shortening the treatment time, such as 5.0 MPa/25°C/5 min (**Fig.**
508 **6a**). These findings suggest that CO₂ gas treatment would have an ideal exposure time, in
509 which ODTs can disintegrate within 20 s, and this time can be shortened by raising CO₂
510 pressure. At 4.0 MPa conditions, the increase in hardness almost reached a plateau after 60
511 min, suggesting that the delay in disintegration profile after 60 min might correlate with the
512 saturation of inter-granule bridging by AMCE.

513

514 3.3.3. Control of physical properties of ODTs at 3.5 MPa conditions

515 Our findings in **Fig. 6** show that 3.5 MPa of CO₂ gas is preferable for this system when using
516 AMCE, as treatment for 180 min maintained rapid disintegration within 15 s and exhibited
517 moderate increases in hardness profile, which would help control the physical properties of
518 ODTs in commercial manufacturing. In this study, the control of physical properties of ODTs
519 using a fixed pressure condition was evaluated.

520 B-1 tablets were treated with CO₂ gas at 20, 25 and 30°C at 3.5 MPa and the effects on
521 physical properties of ODTs were evaluated (**Fig. 7**). Our results demonstrated that tablet
522 hardness of 40–50 N and disintegration of approximately 15 s were reproducibly obtained for
523 the three different temperature conditions (**Figs. 7a, b and c**). These results suggest that the
524 properties of ODTs are well controlled within the temperature range of $25 \pm 5^\circ\text{C}$. A model
525 condition for this ODT system might therefore be 3.5 MPa/25°C/180 min, by simply
526 controlling treatment time, temperature and CO₂ pressure. These conditions would be
527 acceptable as an alternative method for heating or humidifying systems. However, treatment
528 with CO₂ gas for 360 min tended to delay disintegration at 25 and 30°C, which suggests an
529 unfavorable processing time of longer than 180 min. The above conditions consist of a mild
530 temperature of approximately 25°C and a gaseous state of CO₂, which could be obtained
531 using a simple apparatus consisting of a pressure-resistant container connected to a CO₂
532 cylinder. Such a system would enable the easy control of CO₂ pressure introduced into the
533 container *via* adjustment of the pressure valve and temperature. This simplified system would
534 also be beneficial from a commercial perspective because the lack of a heating process at a
535 large production scale would result in lower overall energy costs.

536 These findings demonstrate that the physical properties of ODTs were well controlled by
537 adjusting the pressure of CO₂ gas and temperature in this hardness-enhancing system using
538 AMCE and CO₂ gas.

539

540 *3.4. Effect of AMCE content on physical properties of ODTs*

541 In the present ODT system, the content of AMCE is expected to affect the physical properties
542 of ODTs, in addition to treatment conditions. We therefore evaluated the relationship
543 between AMCE content and the physical properties of ODTs (hardness and disintegration).
544 Formulations are shown as B-1, B-2, B-3, and B-4 (**Table 3**), in which AMCE content
545 increased from 2.5% to 12.5%. The physical properties of ODTs after treatment with CO₂ gas
546 (4.0 MPa/25°C/45 min) were evaluated, and results are shown in **Figs. 8a and b**. In the
547 previous section, 3.5 MPa/25°C/approximately 180 min was suggested as a model condition
548 for preparing ODTs. This experiment, however, was conducted at 4.0 MPa/25°C/45 min, as
549 the B-1 formula under these conditions exhibited similar hardness and disintegration
550 properties to those under the model conditions (**Fig. 6**), which enabled the effects of AMCE
551 content to be compared. Results showed that increases in hardness were content-dependent,
552 and a proportional relationship was confirmed ($R^2=0.9083$) between the increment in
553 hardness and AMCE content (**Fig. 8a**).

554 Regarding disintegration properties (**Fig. 8b**), rapid disintegration of less than 20 s was
555 observed for formulations with AMCE content of 10% or lower. In contrast, the B-4 formula
556 containing the highest AMCE content of 12.5% took longer than 120 s to disintegrate (data
557 not shown). This might be due to excess conditions with regard to both the amount of AMCE
558 and CO₂ treatment, which would delay the disintegration of ODTs. However, this result does
559 not necessarily suggest that the B-4 formula is unacceptable for ODTs, as it exhibited a
560 hardness higher than 50 N and rapidly disintegrated upon processing at lower pressure (3.5
561 MPa/25°C/45 min, **Table 4**). The delayed disintegration of the B-4 formulation was therefore
562 attributed to both bridging agent content and CO₂ gas treatment conditions, with 12.5%
563 AMCE content considered excessive for treatment at 4.0 MPa/25°C/45 min. As shown in **Fig.**

564 **6a and 6c**, formulation with 10% of AMCE required 5.0 MPa to achieve a hardness of higher
565 than 50 N, and this pressure gives only 5 min of preferred time for rapid disintegration.
566 However, as mentioned above, formulation with 12.5% at AMCE provided a hardness of
567 higher than 50 N and rapid disintegration by 3.5 MPa/25°C/45 min, which demonstrates that
568 increasing the amount of AMCE is an effective way of prolonging the preferred treatment
569 time to achieve rapid disintegration while maintaining target hardness. These findings
570 highlight the importance of a balance between the content of the bridging agent and
571 processing conditions in controlling the physical properties of ODTs in this system.

572

573 *3.5. Approaches for controlling physical properties of ODTs*

574 Three different approaches to increasing the tablet hardness of ODTs utilizing high-pressure
575 CO₂ gas under ambient temperature were tested, as follows: increasing the pressure of CO₂,
576 extending the processing time, and increasing AMCE content in the tablet formulation.
577 However, the excessive use of these conditions can also delay the disintegration of ODTs.
578 The general goal of formulating ODTs is to achieve both high hardness and rapid
579 disintegration. It is therefore meaningful to determine which of these approaches is more
580 effective for improving the balance of the physical properties of ODTs.

581 Here, five models of ODTs were prepared based on different input factors, as follows: AMCE
582 content, CO₂ pressure, and CO₂ treatment time. Tablet hardness and disintegration time were
583 compared as output profiles. The ratio of hardness to disintegration (H/D) was set as a
584 parameter (**Table 4**). In general, ODTs with high hardness and rapid disintegration are
585 preferable for commercial products, and H/D is therefore a simple parameter for evaluating
586 the performance of ODTs, in which a higher H/D indicates better performance. As a
587 preliminary experiment, we confirmed that tablets of 19 commercial ODTs in Japan had
588 diameters of 8.5 mm and a mean hardness of 56 N (data not shown). In addition, Yoshita *et al.*

589 (2013) evaluated the disintegration time of 26 commercial ODTs by Tricorptest, with
590 disintegration times ranging from approximately 10 to 30 s and a mean of 20 s. Based on
591 these findings, the expected H/D for commercial ODTs with an 8.5-mm diameter is 2.8 N/s
592 (56 N/20 s).

593 Model 1, which contained 10% AMCE and was processed with CO₂ at 4.0 MPa/25°C/45 min,
594 was used as a control (H/D = 2.8). Models 2 and 3 contained the same polymer content, but
595 had different CO₂ pressurization conditions from Model 1. Model 2 was processed using a
596 higher pressure and shorter time, and the sample had an H/D of 2.6 N/s. Model 3 was
597 processed with a lower pressure and a longer treatment time, and had an H/D of 3.5 N/s,
598 which was higher than that of Model 1. These results suggest that lower pressure conditions
599 help to obtain high H/D ODTs and that a longer processing time does not decrease H/D as
600 much as lowering pressure. This correlates with the discussion above, which is the finding
601 that higher CO₂ pressure made the preferred treatment time shorter to obtain rapid
602 disintegration, and such approach does not increase H/D. However, an approach using a
603 narrow range of treatment times to control the physical properties of ODTs is not suitable for
604 commercial manufacturing. Regarding Models 4 and 5, the physical properties of ODTs were
605 controlled by changing the AMCE content. Model 4 contained a lower polymer content and
606 was processed using a higher CO₂ pressure, which showed an H/D of 1.1 N/s and it was
607 lower than that of Model 1. In contrast, Model 5 showed an H/D of 3.8 N/s, which had a
608 higher AMCE content but was treated with a lower CO₂ gas pressure.

609 These results suggest that the delay in ODT disintegration due to longer CO₂ processing or
610 higher AMCE content can be avoided by decreasing CO₂ pressure, resulting in ODTs with
611 high H/D. In contrast, increasing the CO₂ pressure runs the risk of delaying disintegration and
612 lowering H/D, even if the processing time or content of the polymer used as a bridging agent
613 is decreased. We therefore concluded that the control of CO₂ pressure at 3.5 MPa or lower is

614 the most important factor in producing ODTs with AMCE and XPVP which have a high H/D
615 *via* adjustment of treatment time and formulation.

616

617 **4. Conclusion**

618 In this study, we found that the use of high-pressure CO₂ gas effectively increased tablet
619 hardness with AMCE, HPMCAS, and PVP-VA among the various polymeric excipients
620 screened. With XPVP and CMEC, in contrast, high-pressure CO₂ gas treatment only
621 increased tablet thickness, possibly due to swelling of materials during treatment, and
622 decreased tablet hardness. Regarding the formula containing AMCE, treatment with
623 high-pressure CO₂ gas at 4.0 MPa/25°C/10 min reached near comparable hardness as that
624 with heating at 70°C/720 min. CO₂ gas treatment might therefore increase tablet hardness
625 more efficiently and with less thermal stress than heating. The use of a CO₂ gas system might
626 therefore be preferable in terms of both energy and cost. Furthermore, high-pressure CO₂ gas
627 might increase tablet hardness with EC and conventional plasticizers such as TEC more
628 efficiently than with EC alone. In addition to AMCE, HPMCAS, and PVP-VA, a wide range
629 of other polymers might also be candidates for use in this system.

630 Our work confirmed the effect of CO₂ pressure, temperature, treatment time, and AMCE
631 content on the physical properties of ODTs in the present system. Our operational conditions
632 provided a valid way to demonstrate the plasticization of AMCE at lower temperatures than
633 the T_g (at atmospheric condition) using gaseous CO₂. Some CO₂ treatment conditions delayed
634 the disintegration of ODTs as a result of excessive inter-granule bridging by the insoluble
635 AMCE polymer in the tablet. This effect might be related to the swelling seen with XPVP.
636 The tendency toward delayed disintegration was largely observed under conditions of higher
637 CO₂ pressure, longer treatment time, or higher AMCE content. These findings suggest the
638 importance of optimizing treatment conditions to control the physical properties of ODTs in

639 the system. We also noted that an optimized approach to the production of ODTs increased
640 hardness and accelerated disintegration from the viewpoint of H/D. The present system is
641 expected to achieve equivalent H/D to commercial ODTs.

642 To our knowledge, this is the first report to describe an increase in the hardness of ODTs
643 using a water-insoluble polymer and plasticization with high-pressure CO₂ gas. This system
644 might be suitable for drug substances that are rendered unstable by heat or humidity. In fact,
645 we preliminarily confirmed that ODTs containing acetaminophen, famotidine or tamsulosin
646 hydrochloride could be prepared by CO₂ treatment, and showed preferable hardness and
647 disintegration properties (Kobayashi *et al.*, 2013). Further investigation of ODTs containing
648 drug substances are needed to confirm stability, loading capacity and dissolution profiles,
649 which are also important properties of ODTs. Furthermore, our results suggest that this CO₂
650 gas treatment requires a simpler apparatus than supercritical CO₂ systems, as pressure
651 supplied from a CO₂ cylinder is sufficient, without the need for a condensing process. This
652 system might easily be scaled up for commercial purposes. Further modification and a
653 larger-scale study are therefore required to produce ODTs using this technology for
654 pharmaceutical research.

655

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728 **Figure legends**

729 **Figure 1.** Schematic diagram of the experimental apparatus for pressurizing tablets using
730 carbon dioxide. 1, CO₂ source (non-siphon cylinder); 2, pressure regulator; 3, stop valve; 4,
731 thermostatic chamber; 5, pressure-resistant container (50 mL); 6, thermometer; 7, back
732 pressure regulator

733

734 **Figure 2.** Scanning electron microscopy images of polymeric excipients. Intact samples of
735 (a) AMCE, (b) PVP-VA, (c) HPMCAS and (d) CMEC. CO₂-treated samples at 6.0
736 MPa/25°C/45 min (e) AMCE, (f) PVP-VA, (g) HPMCAS and (h) CMEC. CO₂-treated
737 samples at 4.0 MPa/25°C/45 min (i) AMCE and (j) PVP-VA.

738

739 **Figure 3.** Time effect on tablet hardness (a) and tablet thickness (b) by different treatments.
740 Treatment 1: 25°C treatment with CO₂ gas at 4.0 MPa (open circles). Treatment 2: 70°C
741 heating under atmospheric air (closed circles). Sample at 0 min represents the no-treatment
742 sample. Each plot represents mean ± SD (*n*=5) and **P*<0.05, †*P*<0.01, vs. 0 min sample of
743 each treatment method.

744

745 **Figure 4.** Scanning electron microscopy images of AMCE. (a) CO₂ at 4 MPa/25°C/120 min,
746 (b) heated at 70°C/120 min and (c) heated at 70°C/840 min

747

748 **Figure 5.** Effect of CO₂ gas pressure on tablet hardness (a and b), thickness (c) and
749 disintegration time (d) at 15°C (open circles), 25°C (open squares), 35°C (closed circles) and
750 45°C (closed squares). All treatments were conducted for 45 min. x-axis of (a) CO₂ gas
751 pressure converted to CO₂ gas density in (b). †*P*<0.01 vs. 15°C sample at each processing
752 time. Hardness and thickness data represent mean ± SD (*n*=5) and disintegration data are

753 mean \pm SD ($n=3$). Disintegration data at more than 4.0 MPa condition are not shown in (d),
754 as these resulted in disintegration times of more than 120 s for all temperatures.

755

756 **Figure 6.** Effect of pressurizing time by CO₂ gas on tablet hardness (a), thickness (b) and
757 disintegration time (c) under four different pressure conditions, namely 3.0 MPa (open
758 triangles), 3.5 MPa (open squares), 4.0 MPa (closed triangles) and 5.0 MPa (closed squares).

759 All treatments were conducted at 25°C. Hardness and thickness data are mean \pm SD ($n=5$),
760 and disintegration data are mean \pm SD ($n=3$). For 4.0 and 5.0 MPa, the proportion of
761 disintegration data are not shown in (c), as these resulted in disintegration of more than 2
762 min.

763

764 **Figure 7.** Relationship between processing time and physical properties of ODTs, tablet
765 hardness (a), thickness (b) and disintegration time (c). CO₂ gas pressure was set as 3.5 MPa at
766 20°C (open triangles), 25°C (closed circles) and 30°C (open squares). Hardness and thickness
767 data are mean \pm SD ($n=5$), and disintegration data are mean \pm SD ($n=3$).

768

769 **Figure 8.** Relationship between content of AMCE and physical properties of ODTs,
770 increment of tablet hardness (a), and disintegration time (b) after CO₂ treatment at 4.0
771 MPa/25°C/45 min. Hardness data are mean \pm SD ($n=5$), and disintegration data are mean \pm
772 SD ($n=3$). For the 12.5% AMCE content formulation, disintegration data are not shown in (b),
773 as this resulted in disintegration of more than 2 min.

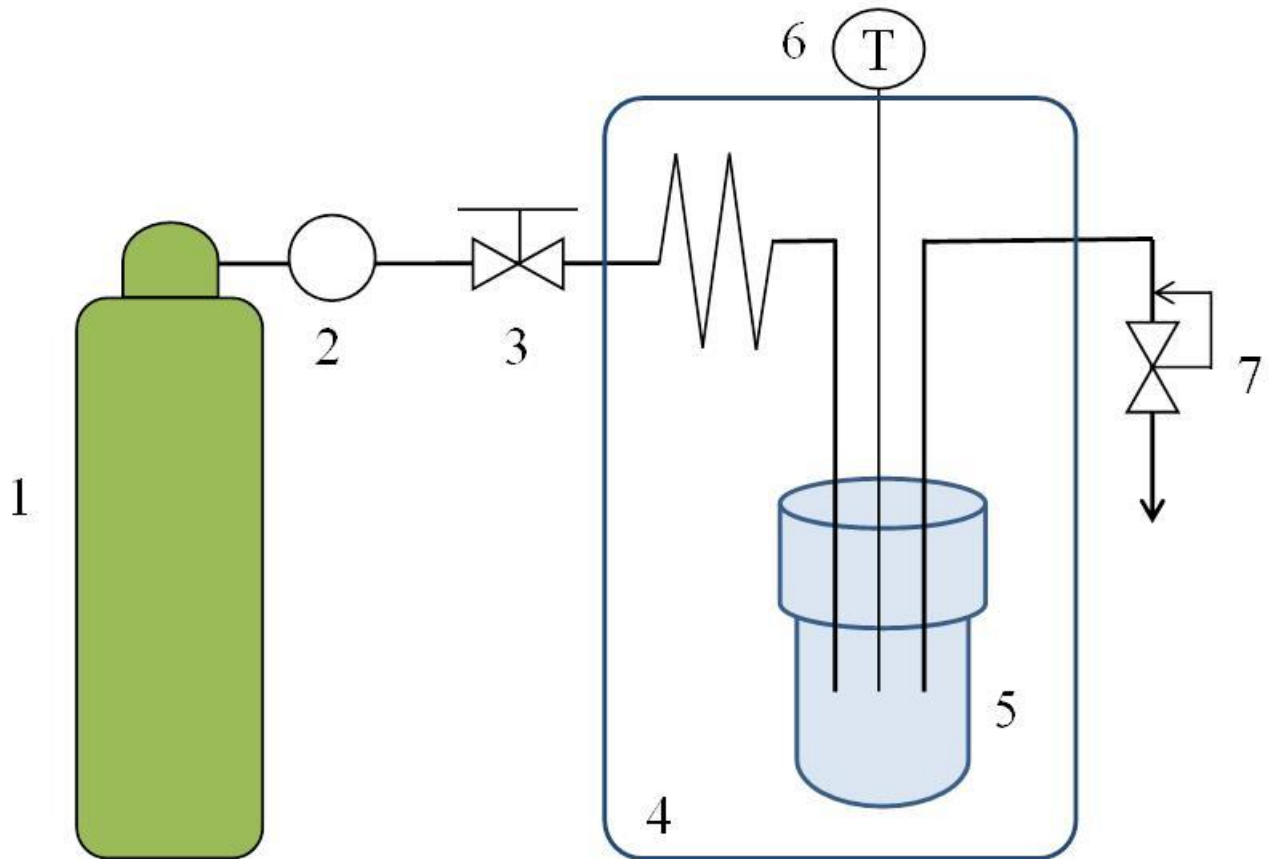
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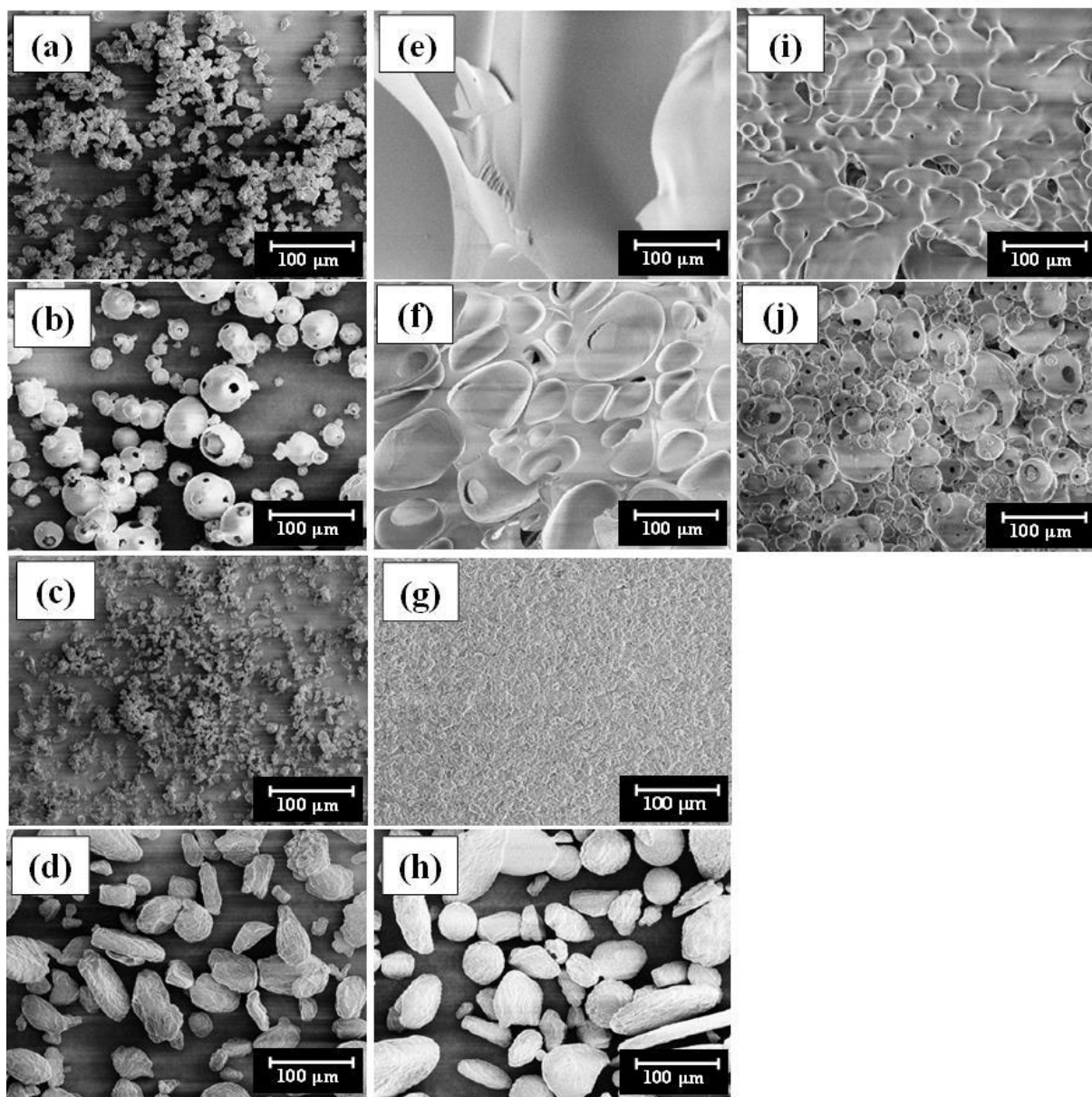
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Figure 1



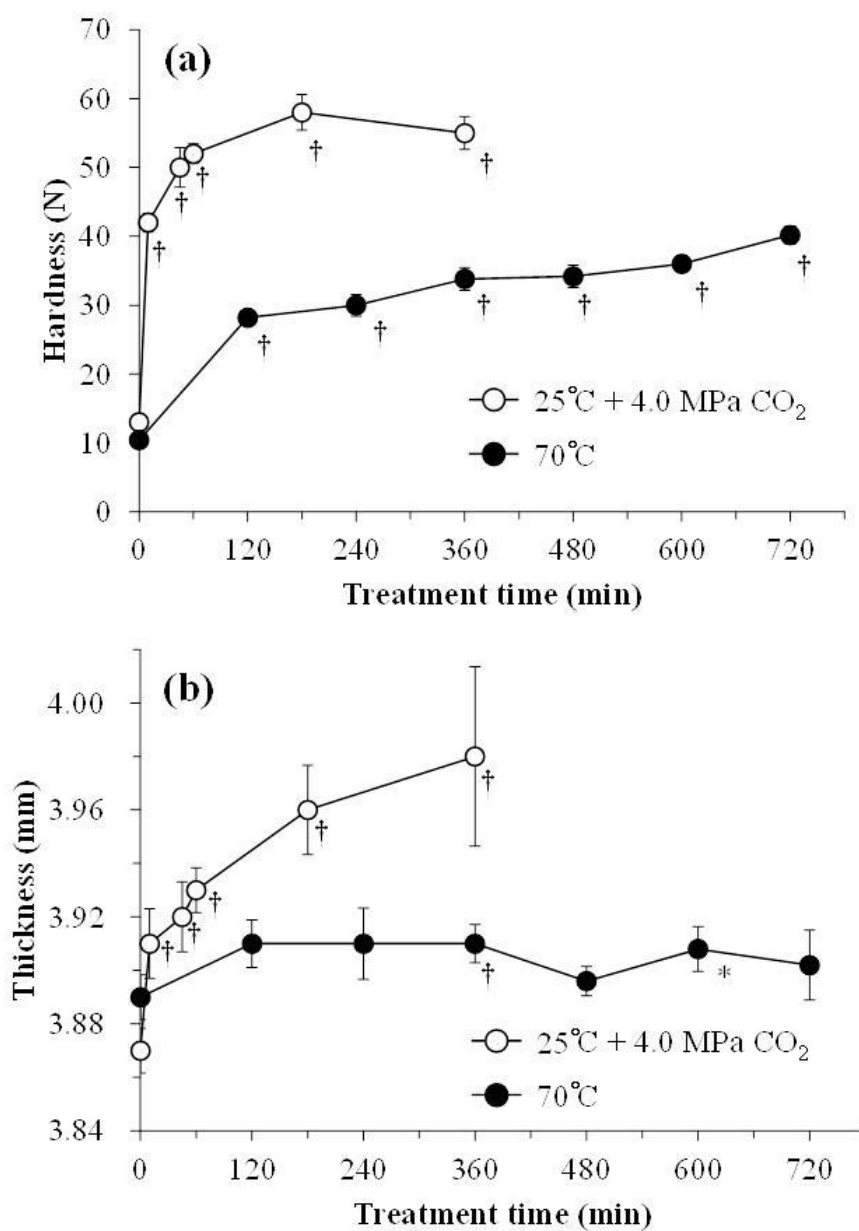
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Figure 2



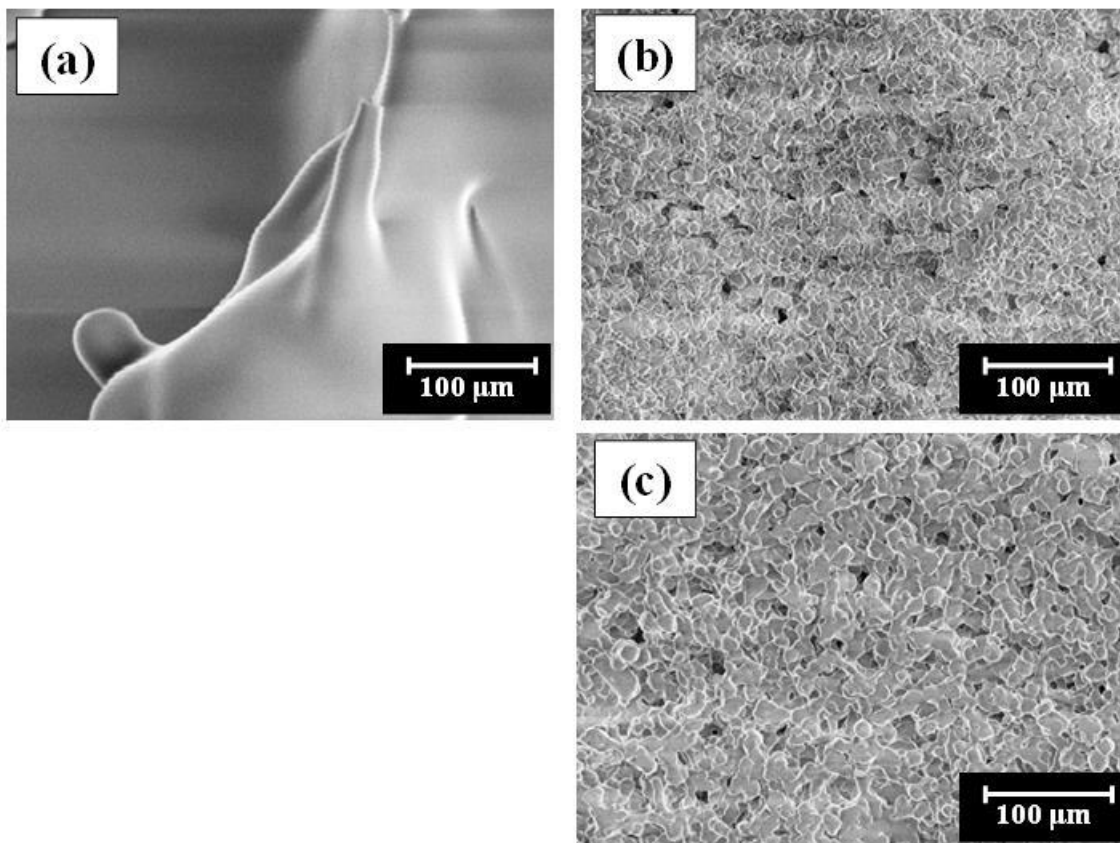
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Figure 3



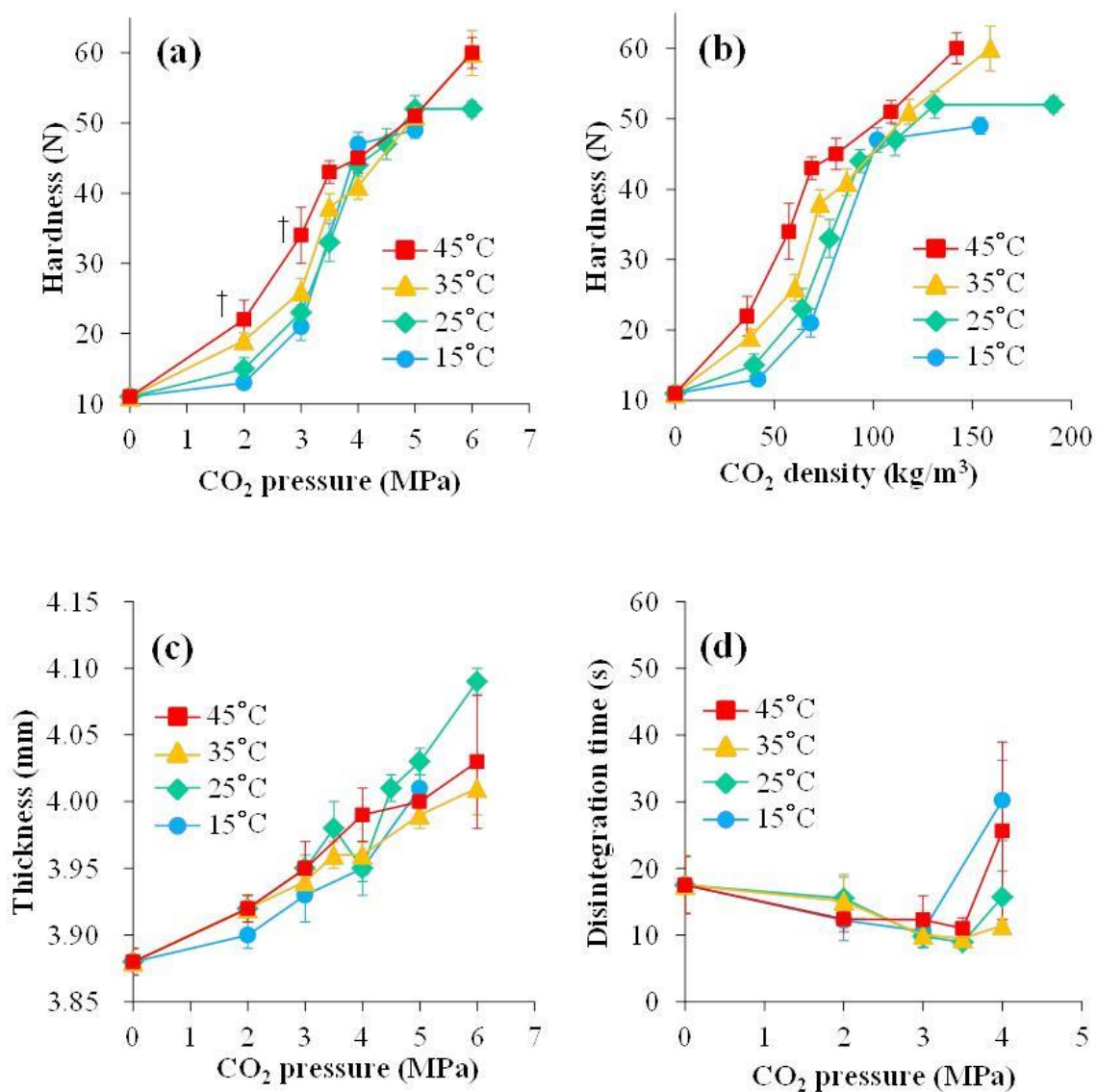
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Figure 4



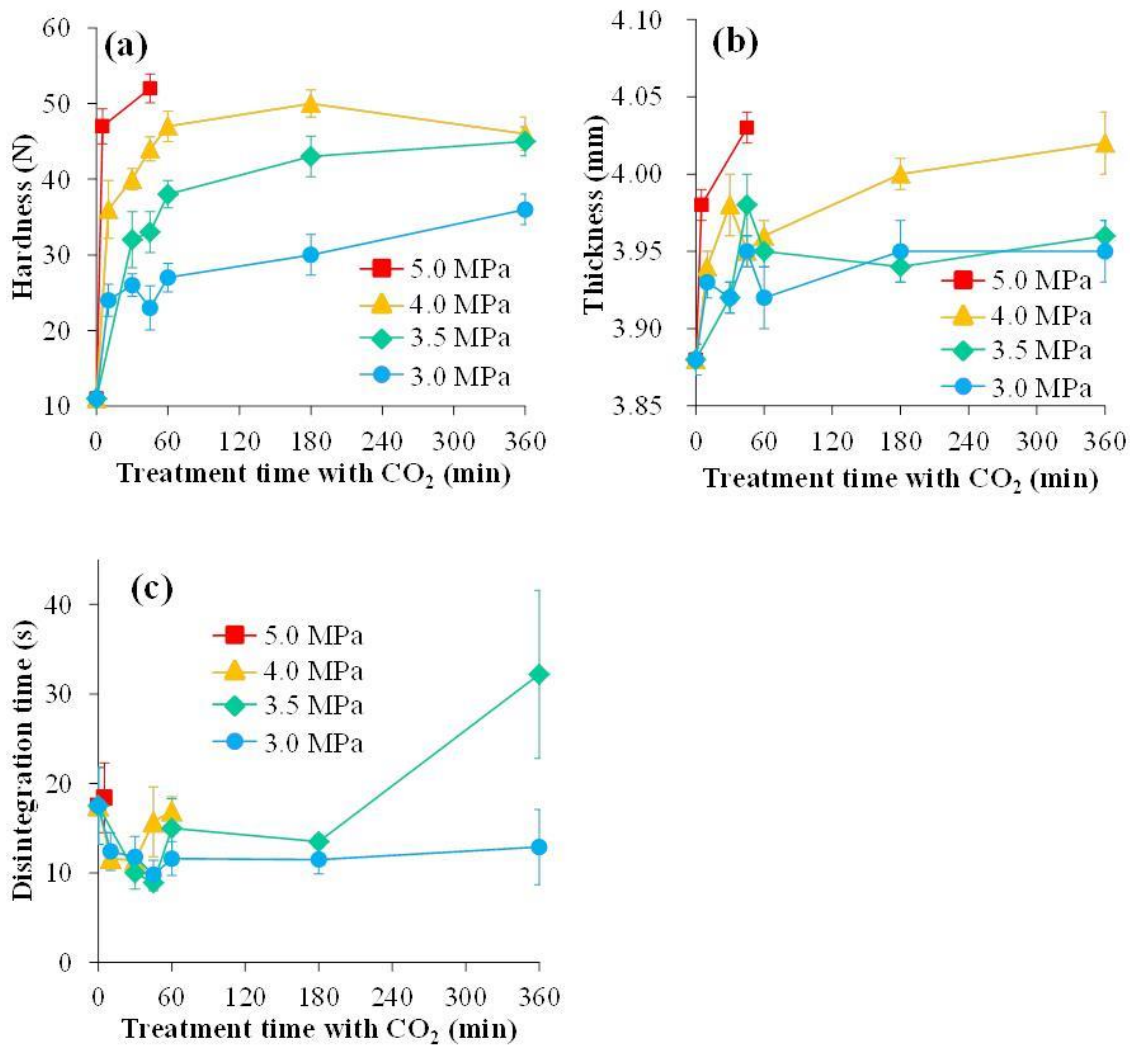
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Figure 5



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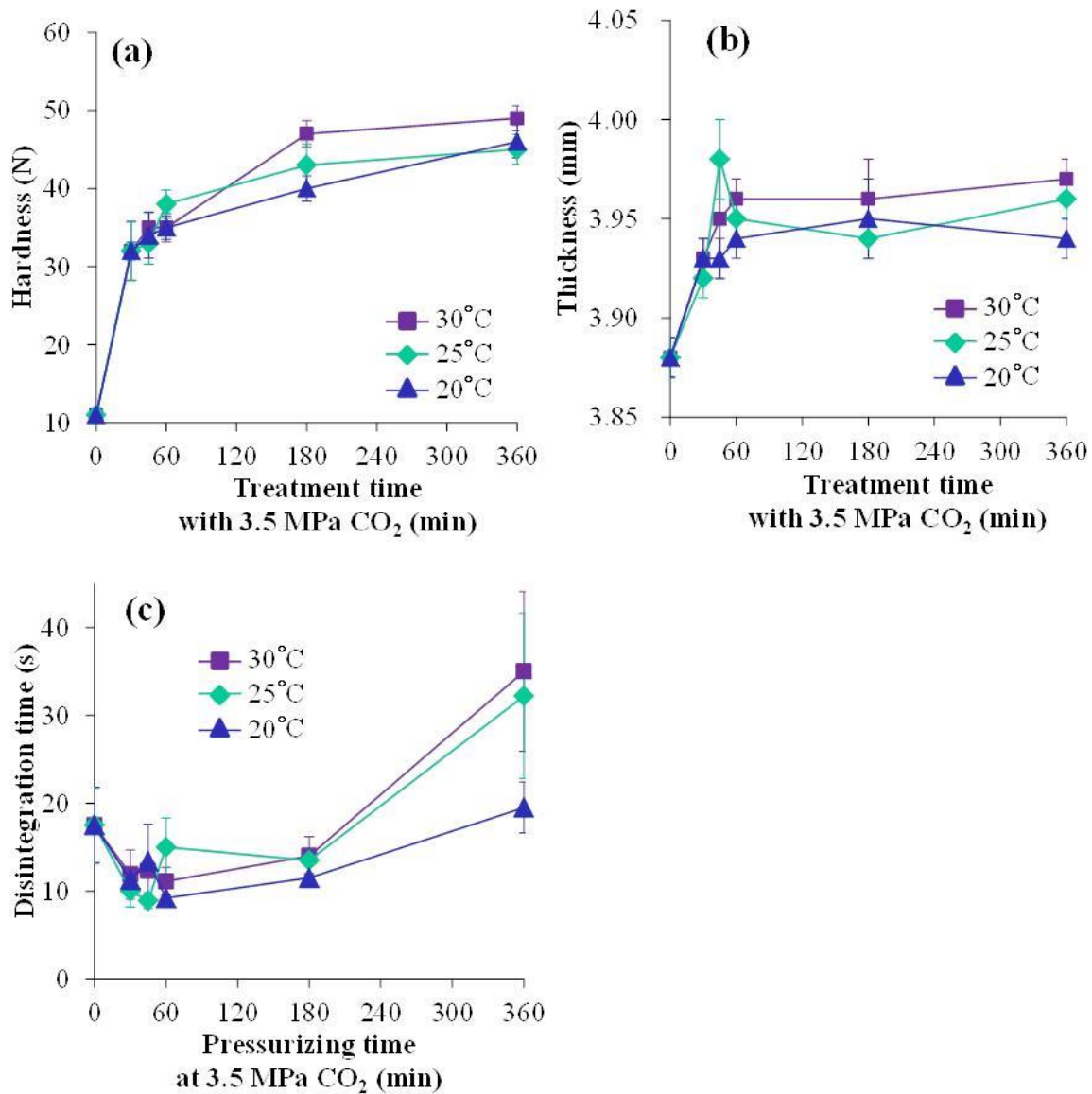
Figure 6



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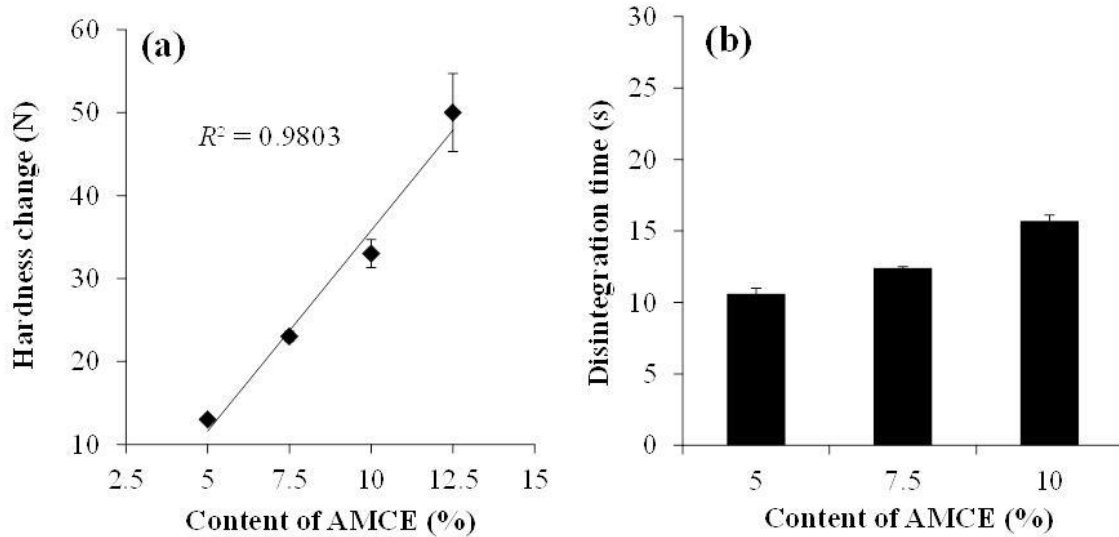
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Figure 7



785

Figure 8



786